



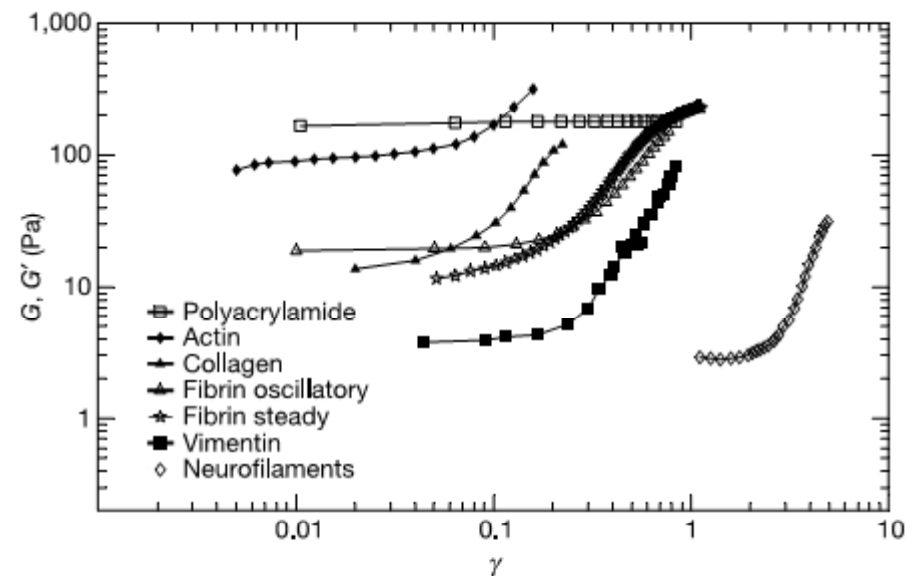
More Non-Linear Rheology

D. Vader

Weitzlab group meeting tutorial

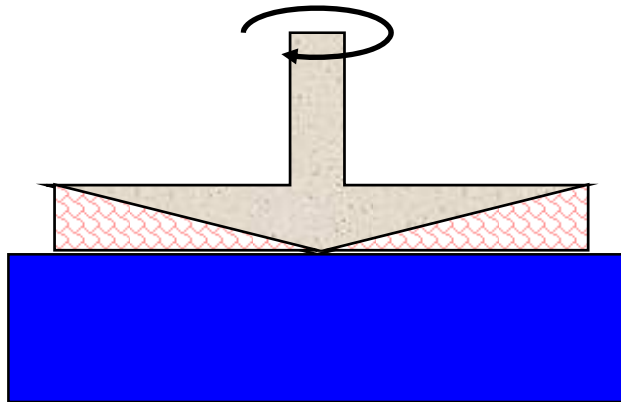
Rheology of biopolymers

- “*Unlike simple polymer gels, many biological materials—including blood vessels, mesentery tissue, lung parenchyma, cornea and blood clots—stiffen as they are strained, thereby preventing large deformations that could threaten tissue integrity.*” (Storm *et al.*, 2005)
- Tensile uniaxial and biaxial tests show similar behavior (Roeder *et al.*, Brightman *et al.*) for collagen type I gels.



Oscillatory Shear in Bulk Rheology

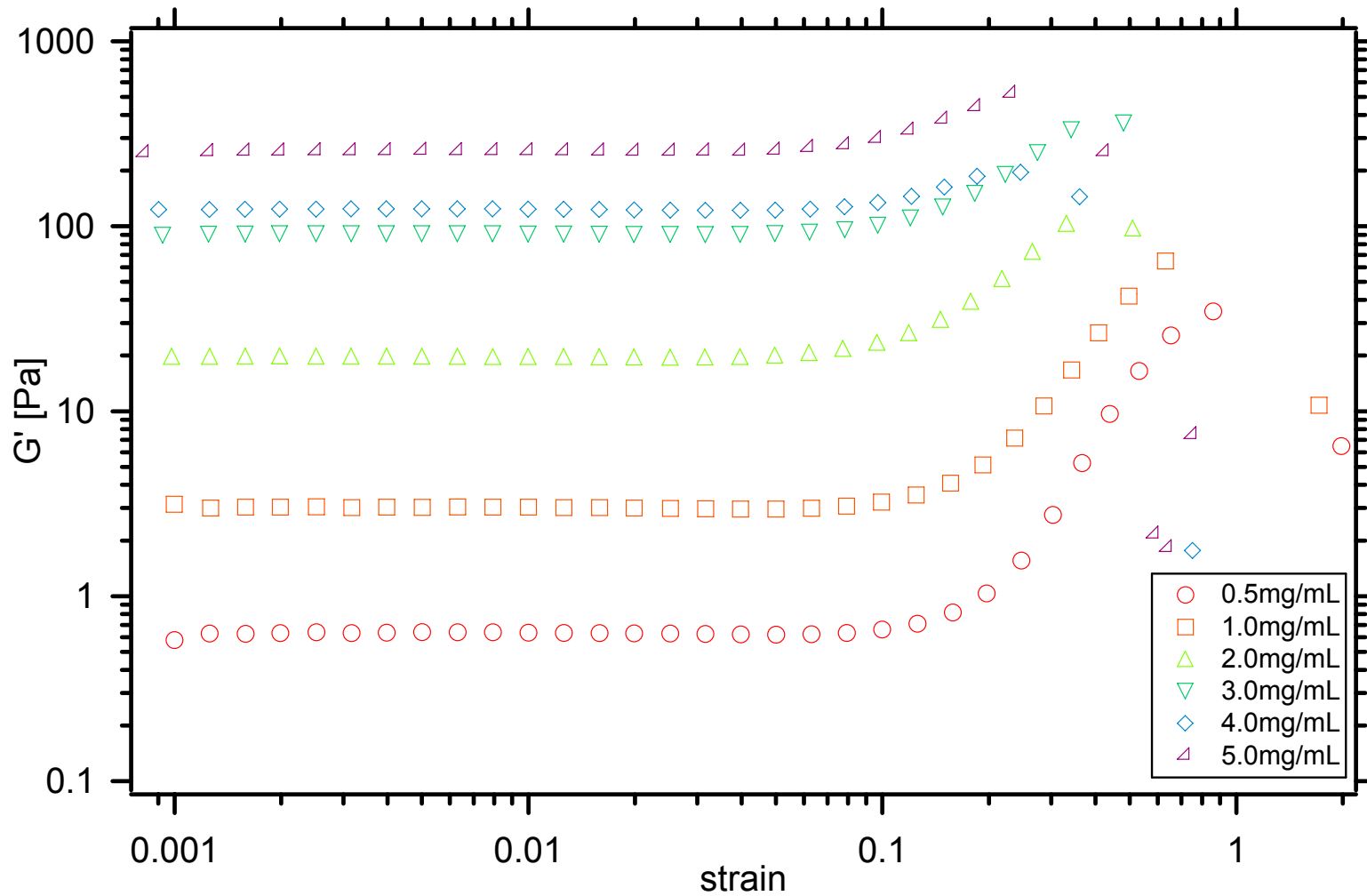
- Advantages
 - Low sample volume
 - Well-controlled geometry
 - Well-characterized methods and protocols



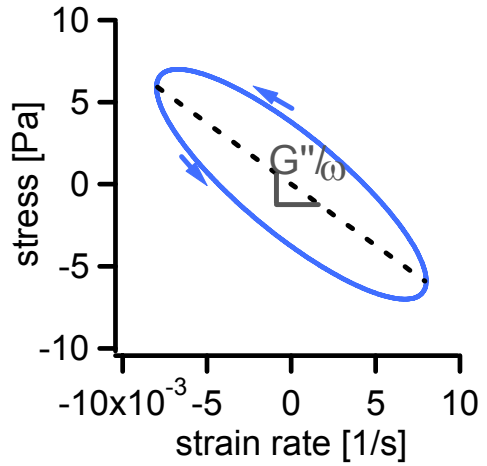
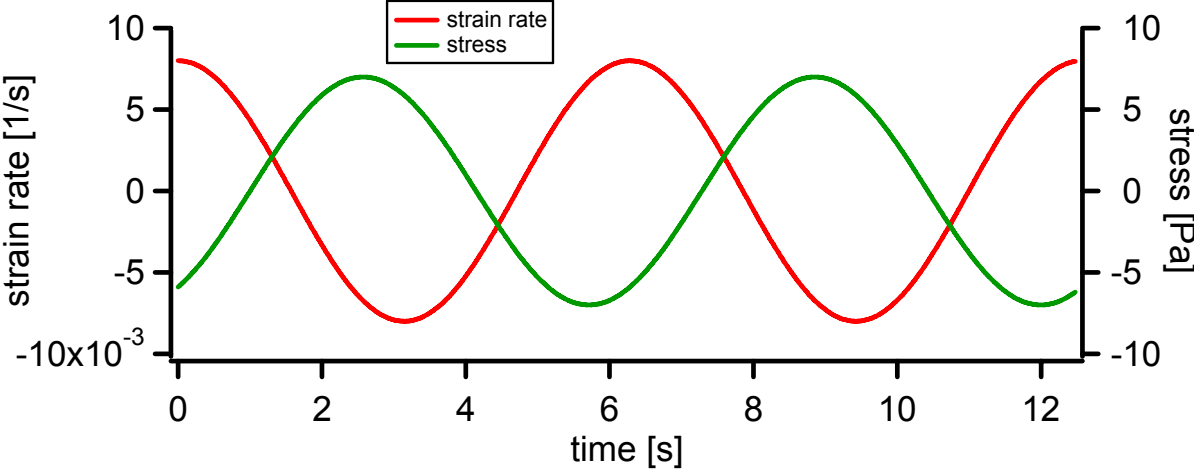
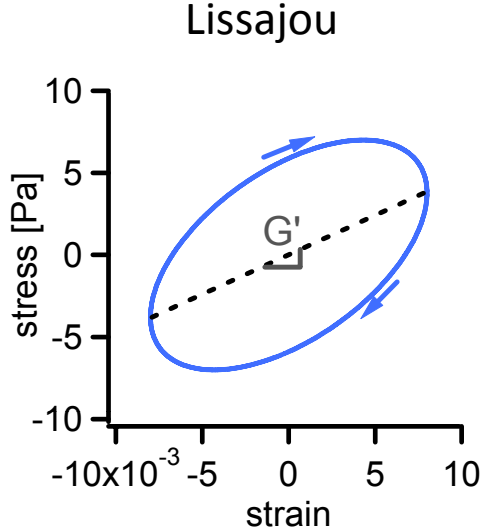
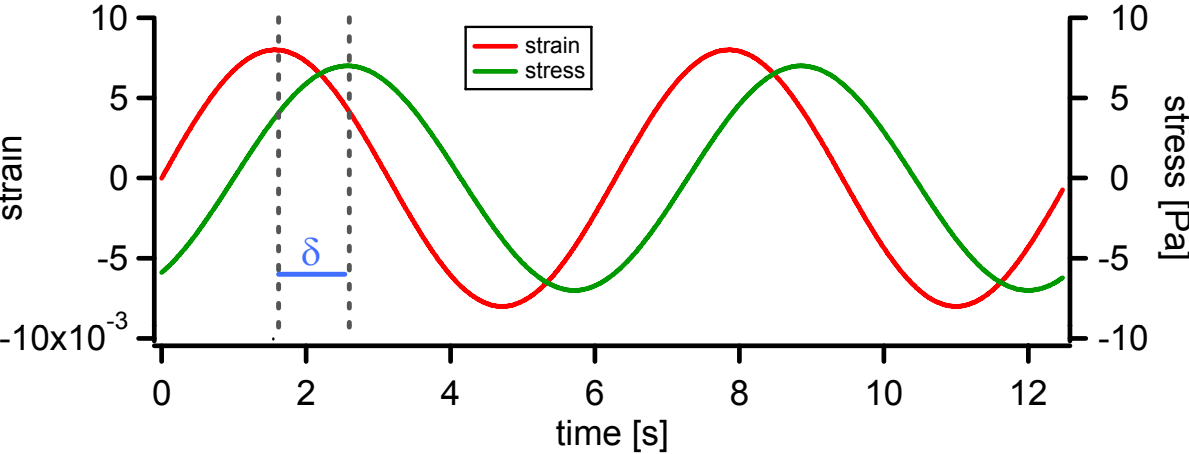
$$\gamma(t) = \gamma_0 \cdot \sin(\omega t)$$

$$\sigma(\omega, t) = G'(\omega) \gamma(\omega t) + G''(\omega) \frac{\dot{\gamma}(\omega t)}{\omega}$$

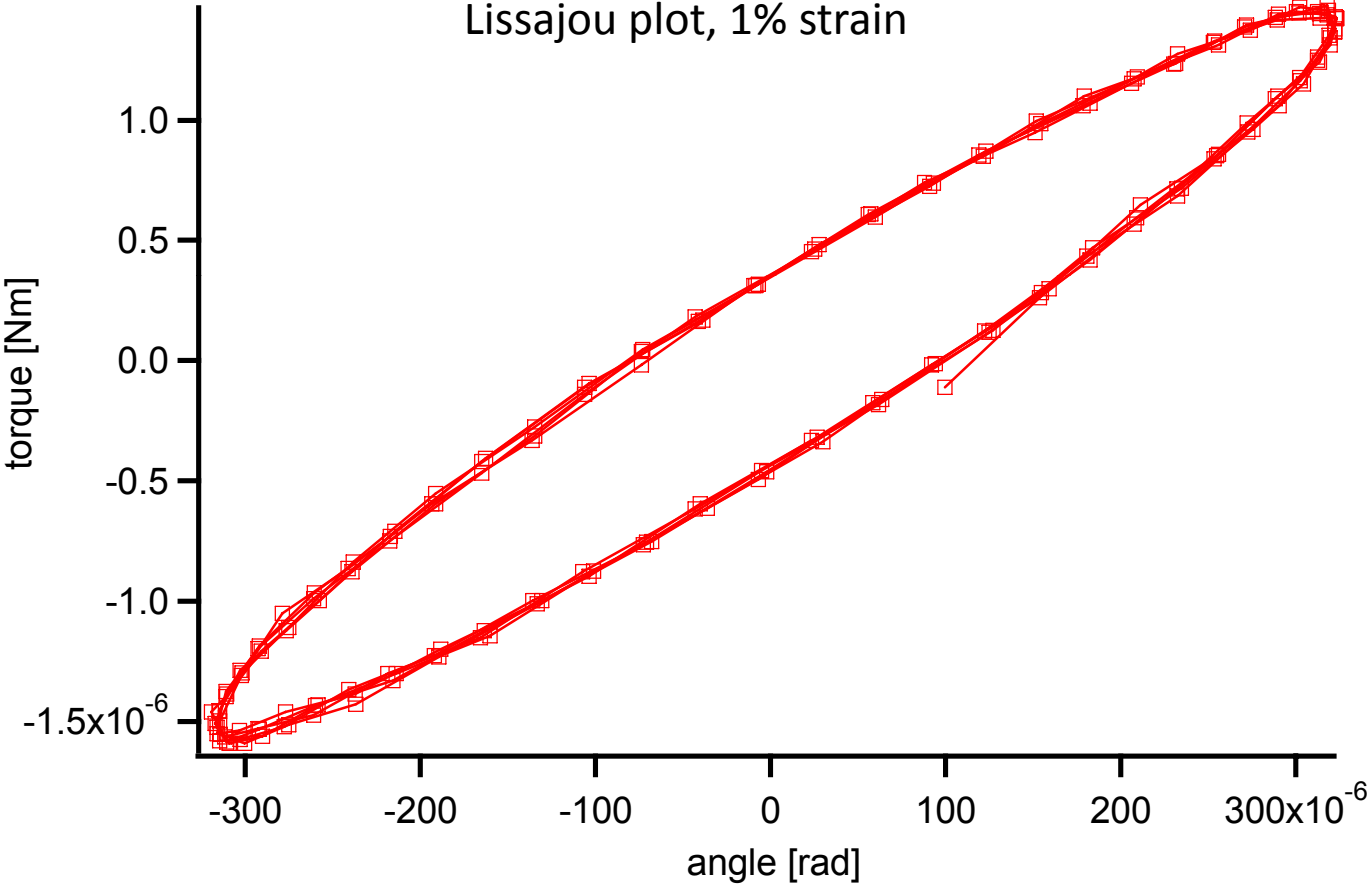
Oscillatory strain sweeps (collagen gels)



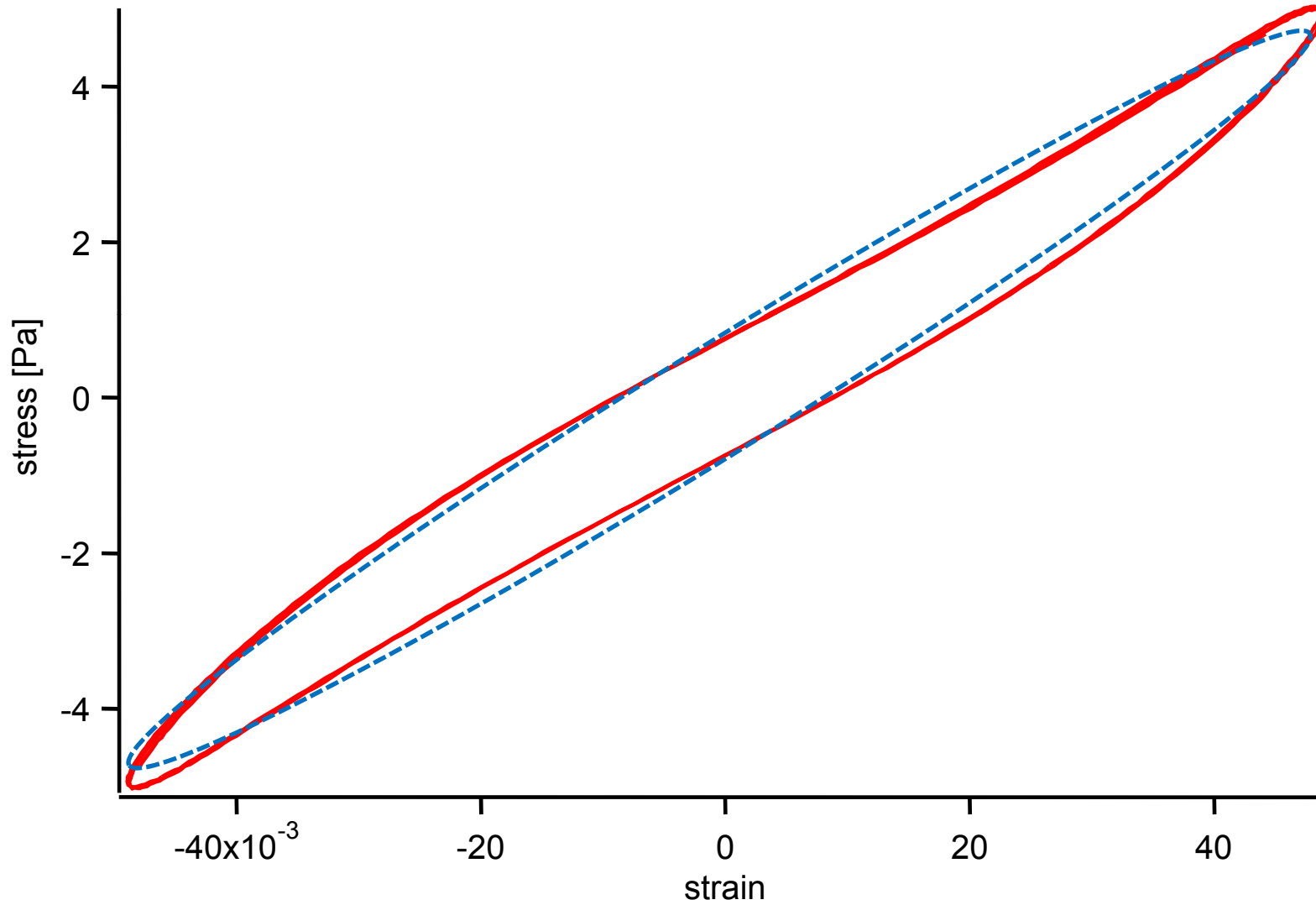
Lissajou plots



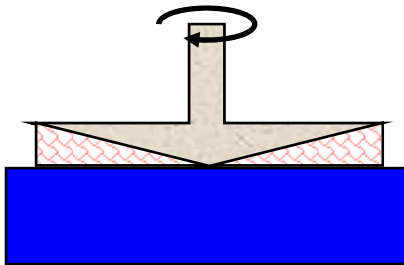
Raw data: Lissajou plots



Nonlinear Lissajou plot

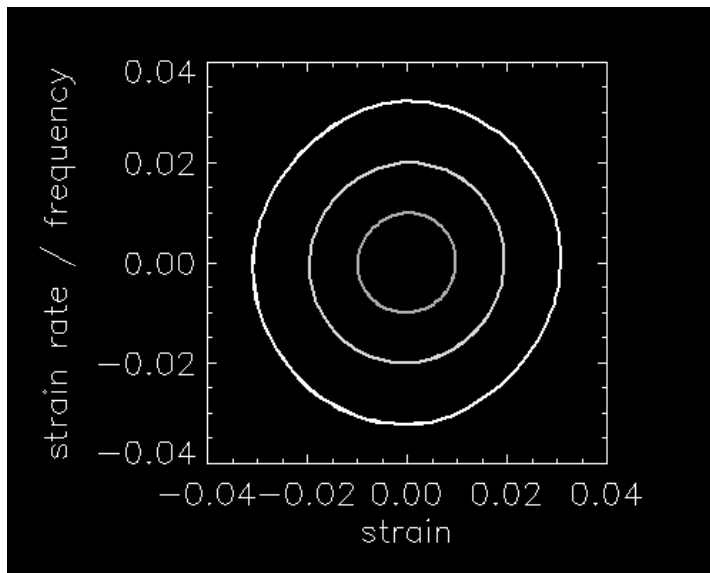


Linear viscoelasticity



$$x = \gamma \text{ and } y = \dot{\gamma}/\omega$$

$$x^2(t) + y^2(t) = \gamma_0^2$$



$$\gamma(t) = \gamma_0 \cdot \sin(\omega t)$$

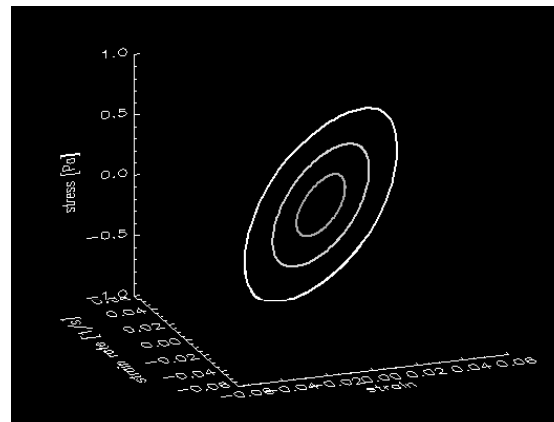
$$\sigma(\omega, t) = G'(\omega) \gamma(\omega t) + G''(\omega) \frac{\dot{\gamma}(\omega t)}{\omega}$$

$$\sigma(x, y) = \sigma'(x, \gamma_0) + \sigma''(y, \gamma_0)$$

$$\sigma' = G' x(t), \quad \sigma'' = G'' y(t)$$

$$\oint \sigma' dx = 0, \quad \oint \sigma'' dy = 0$$

$$\oint \sigma dx = \oint \sigma' dx, \quad \oint \sigma dy = \oint \sigma' dy$$



Normal vector
 $\mathbf{n} = G' \mathbf{i} + G'' \mathbf{j} - \mathbf{k}$

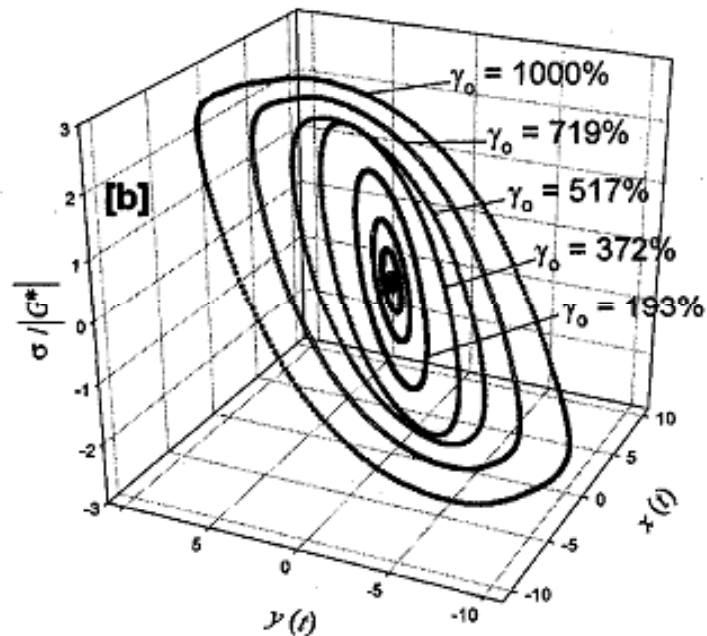
Generalized moduli

$$\sigma' = \Gamma'(x, \gamma_0)x, \quad \sigma'' = \Gamma''(y, \gamma_0)y$$

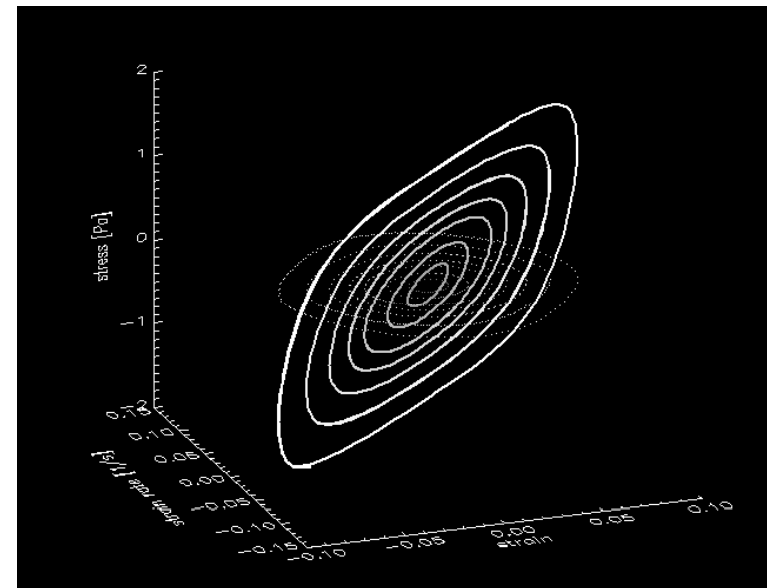
$$\lim_{\gamma_0 \rightarrow 0} \Gamma'(x, \gamma_0) = G'(\omega), \quad \lim_{\gamma_0 \rightarrow 0} \Gamma''(y, \gamma_0) = G''(\omega)$$

$$\sigma'(x, \gamma_0) = G'(\omega)x + G'_3(\omega, \gamma_0)x^3 + G'_5(\omega, \gamma_0)x^5 + \dots$$

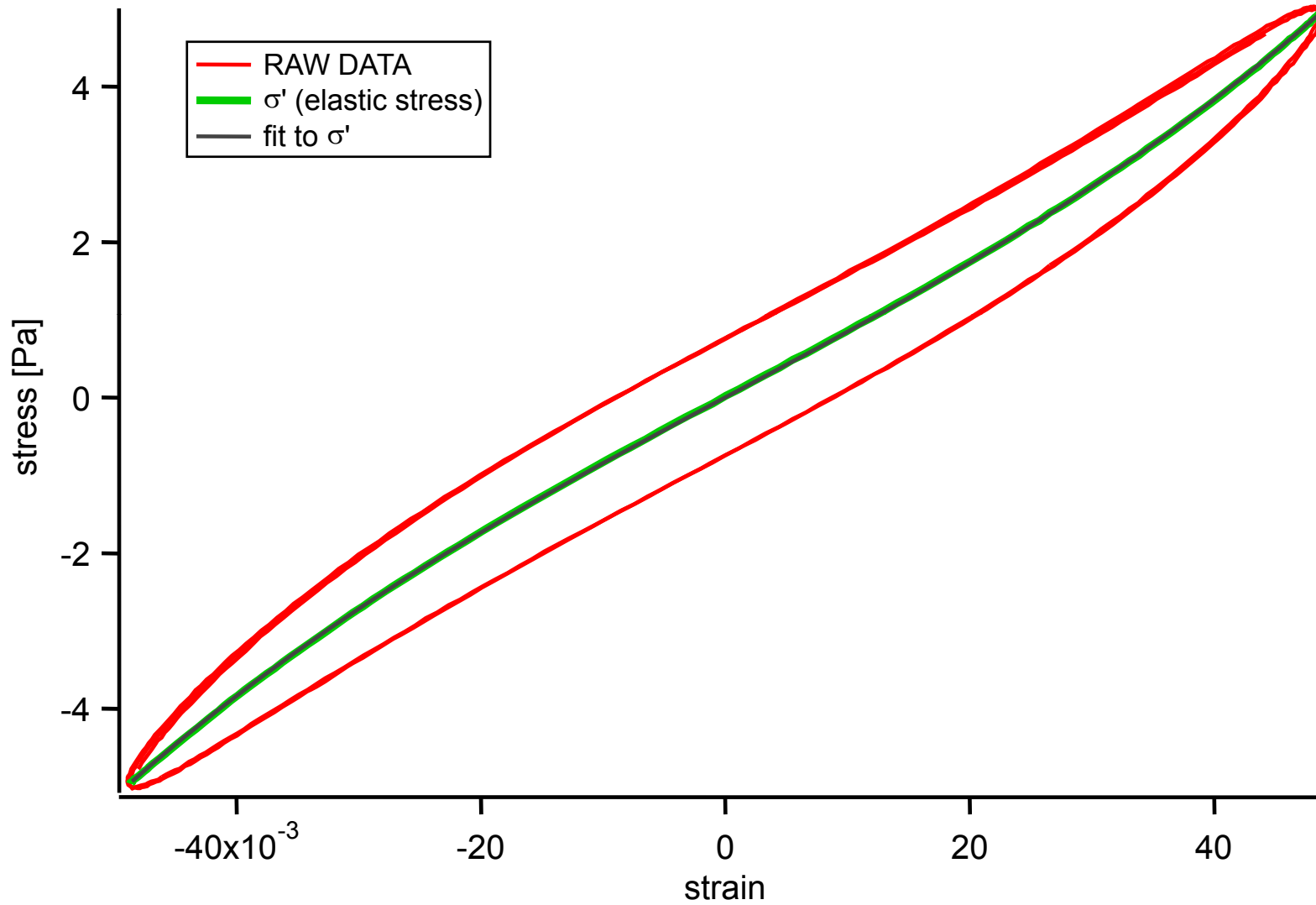
Cho data: shear thinning



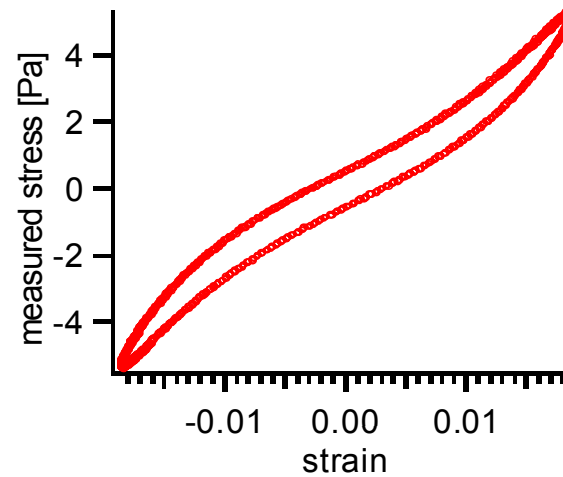
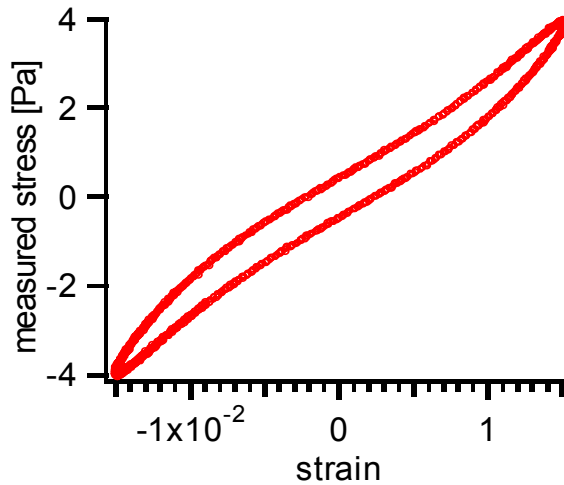
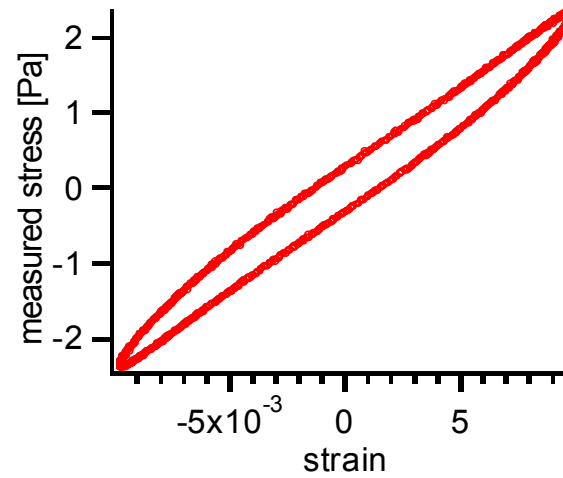
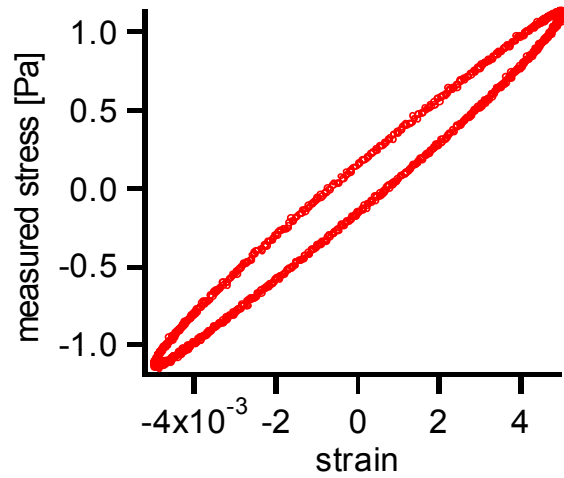
2mg/mL collagen: strain stiffening



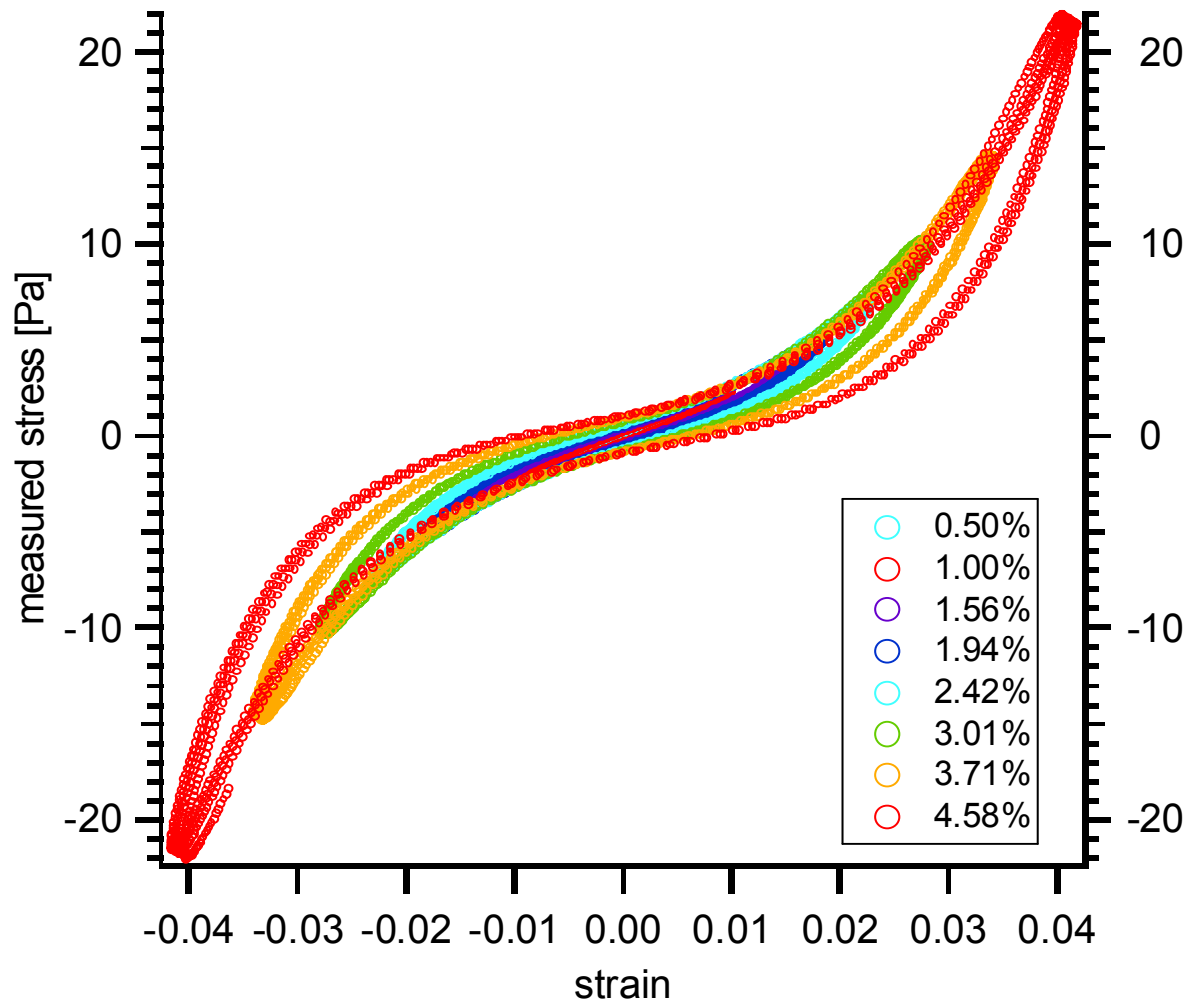
Nonlinear Lissajou plot



2.4mg/mL cone-plate

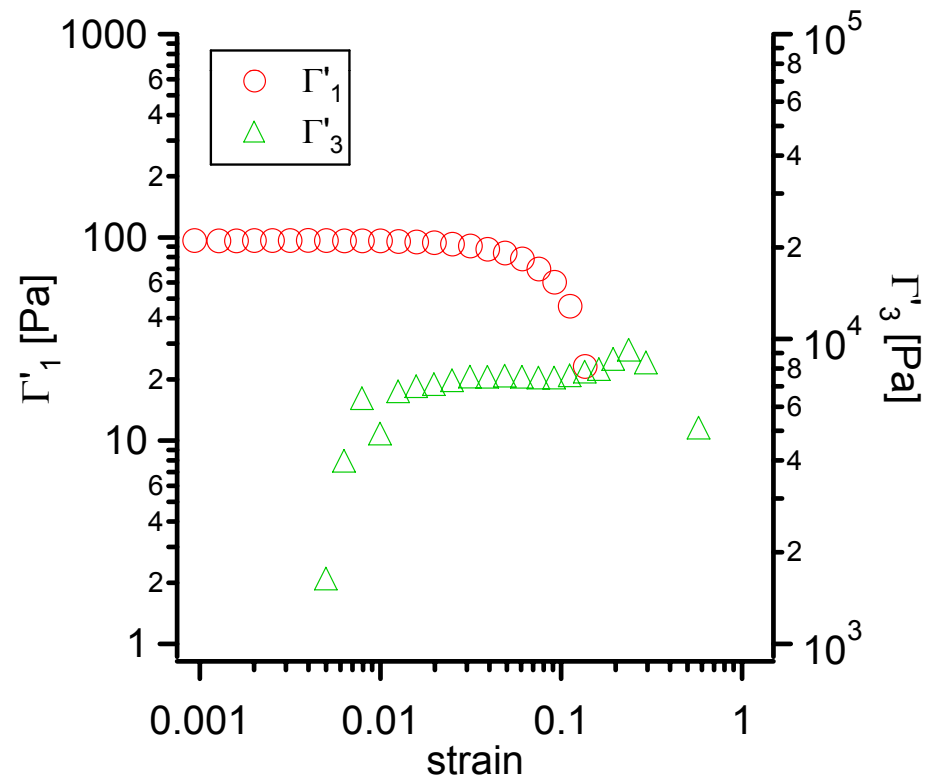
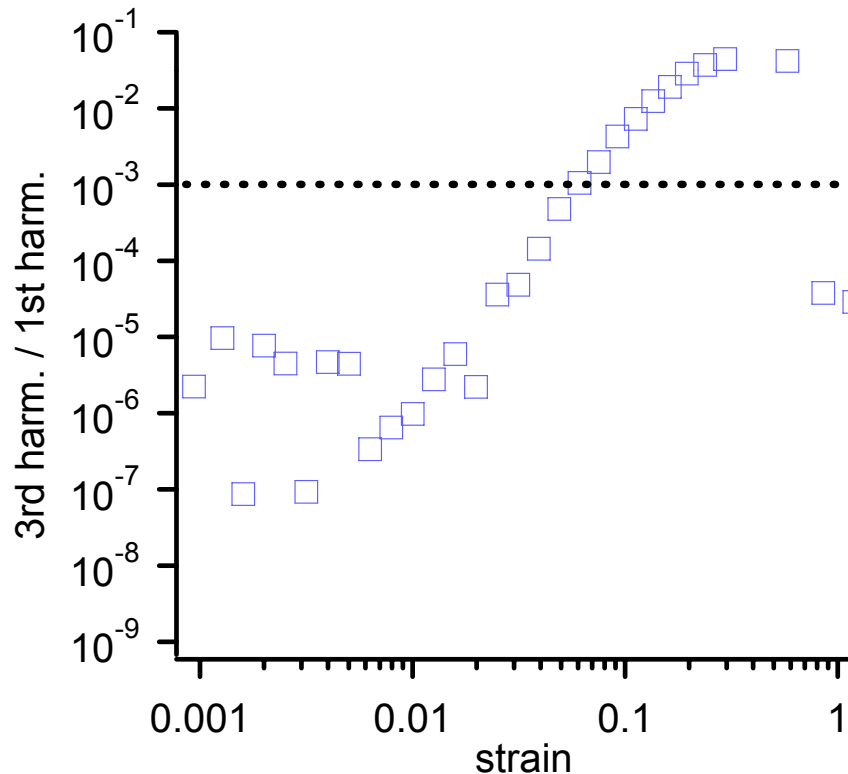


2.4mg/mL cone-plate



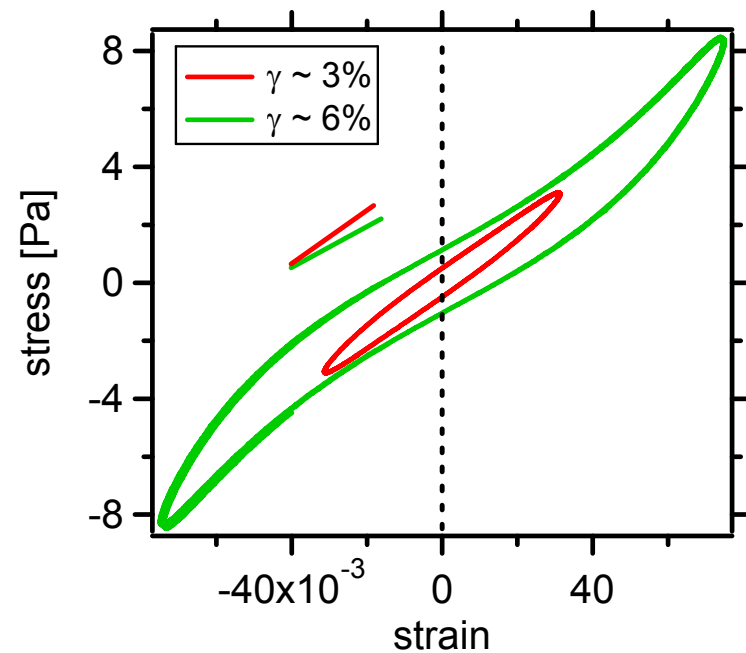
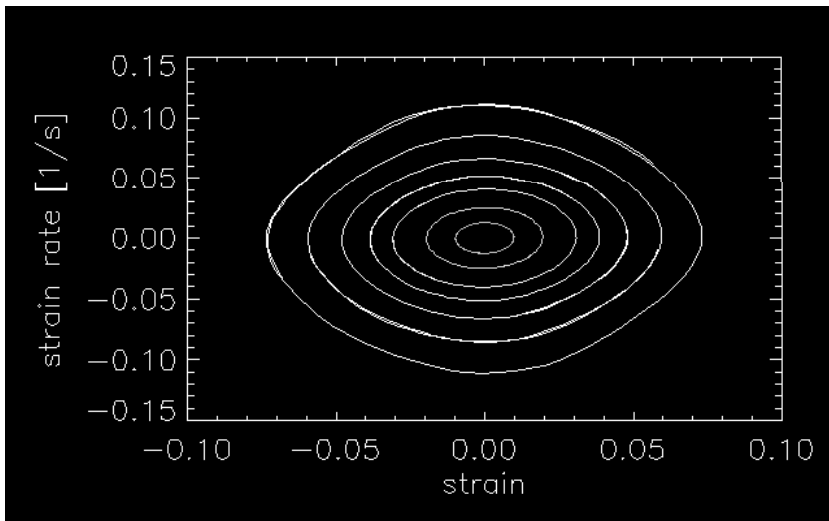
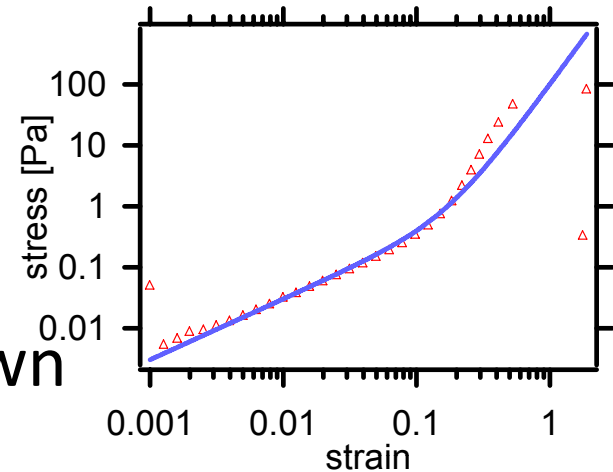
Self-consistency checks

- Frequency spectrum of $\gamma(t)$ should be close to $\delta(f_0)$
- 3rd order polynomial fit done locally, i.e. for each γ :
 - Γ'_1, Γ'_3 consistent over a range of γ ?
 - Can we do a global 3rd order polynomial fit of σ vs γ ?

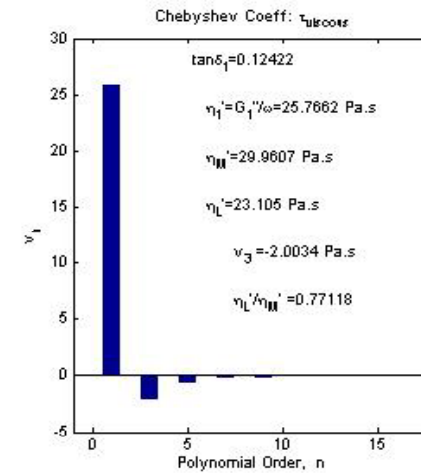
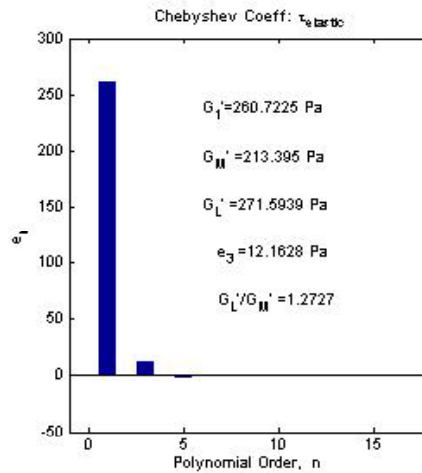
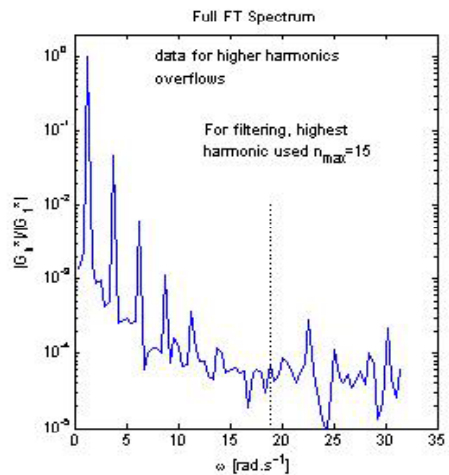
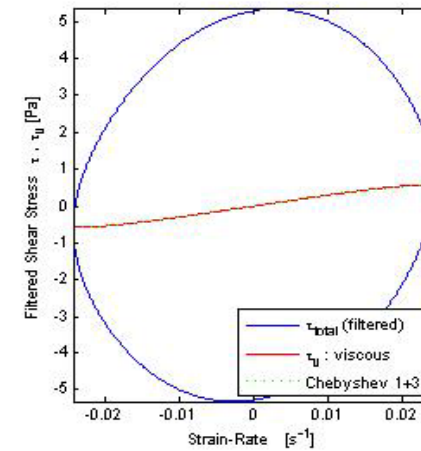
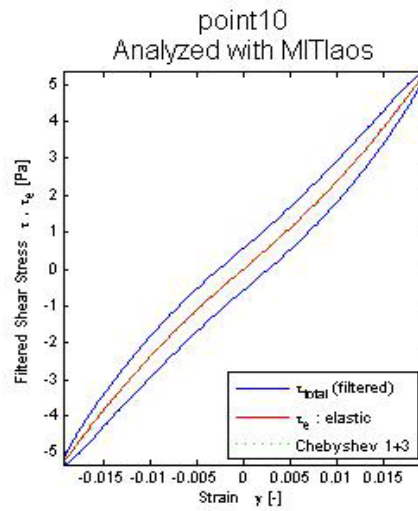
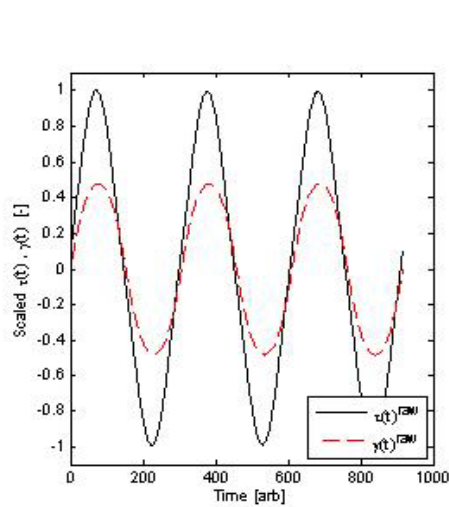


Breakdown of the model

- Low concentrations
- High strains
 - Pseudo-strain control breaks down
 - Higher order terms needed
 - Shear thinning?



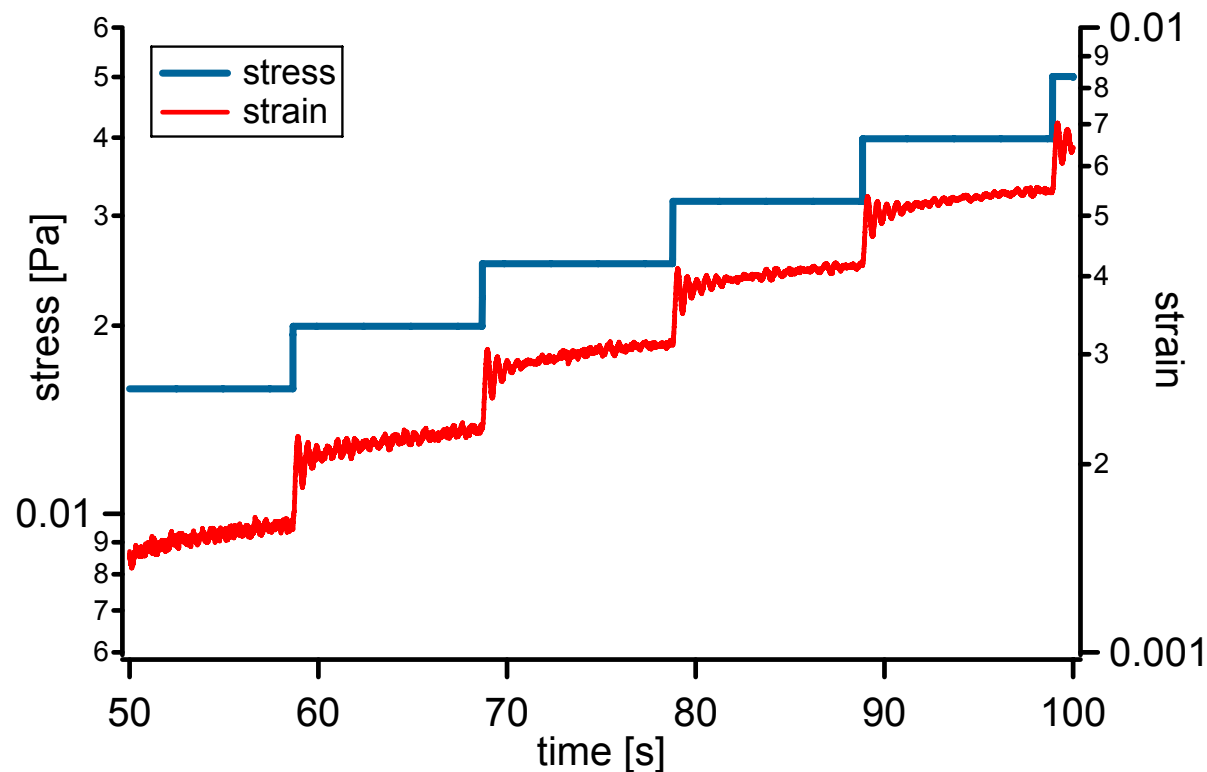
MIT LAOS MATLAB package



Creep-ringing

Creep-ringing

- Norman & Ryan's work here (fibrin, jamming)
- Good tutorial by Ewoldt & McKinley (MIT)



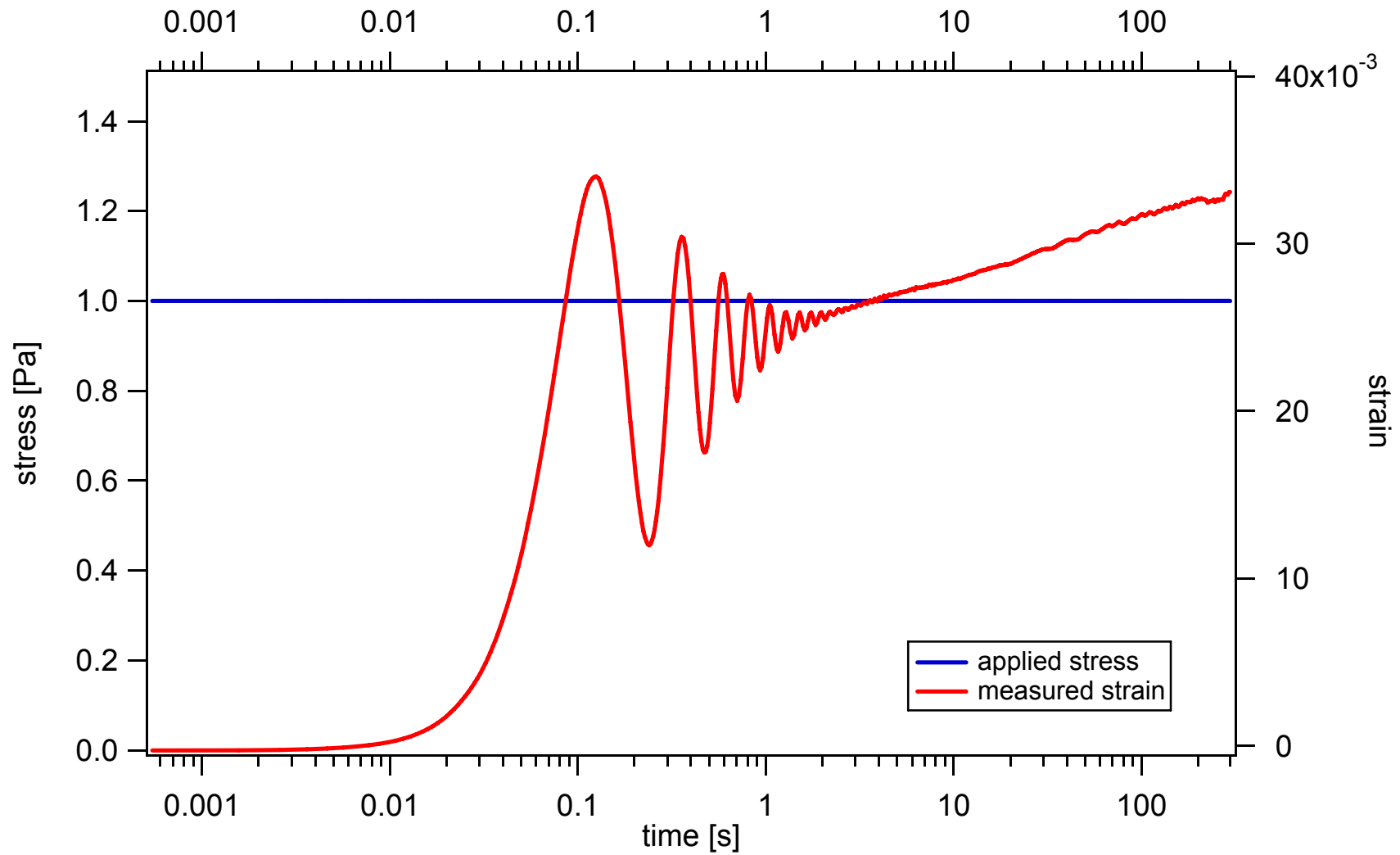
$$G' \approx \frac{I\omega^2}{b} \left(1 + \left(\frac{\Delta}{2\pi} \right)^2 \right)$$

$$G'' \approx \frac{I\omega^2}{b} \left(\frac{\Delta}{\pi} \right)$$

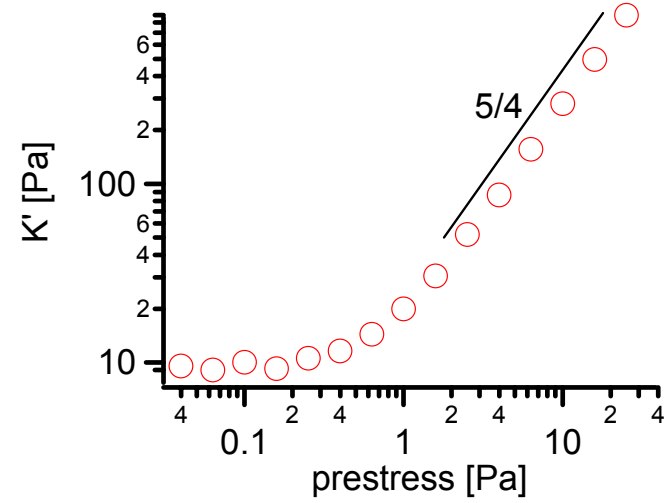
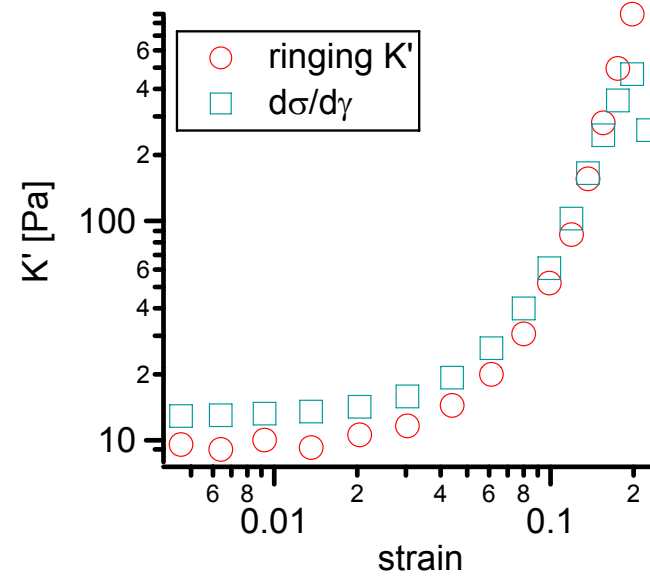
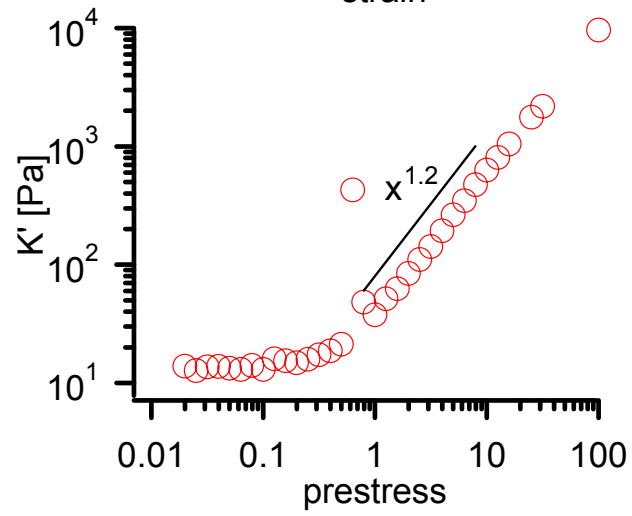
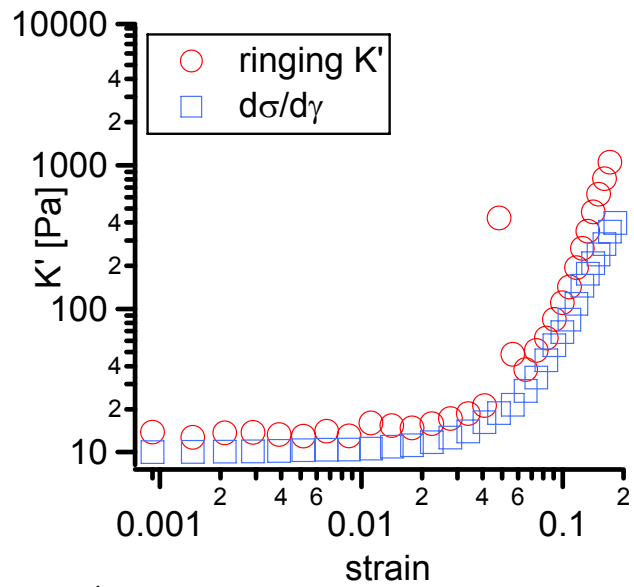
$$\Delta = \frac{1}{n} \ln \left(\frac{A_1}{A_{n+1}} \right)$$

$$b = \frac{2\pi \cdot R^3}{3 \tan \theta}$$

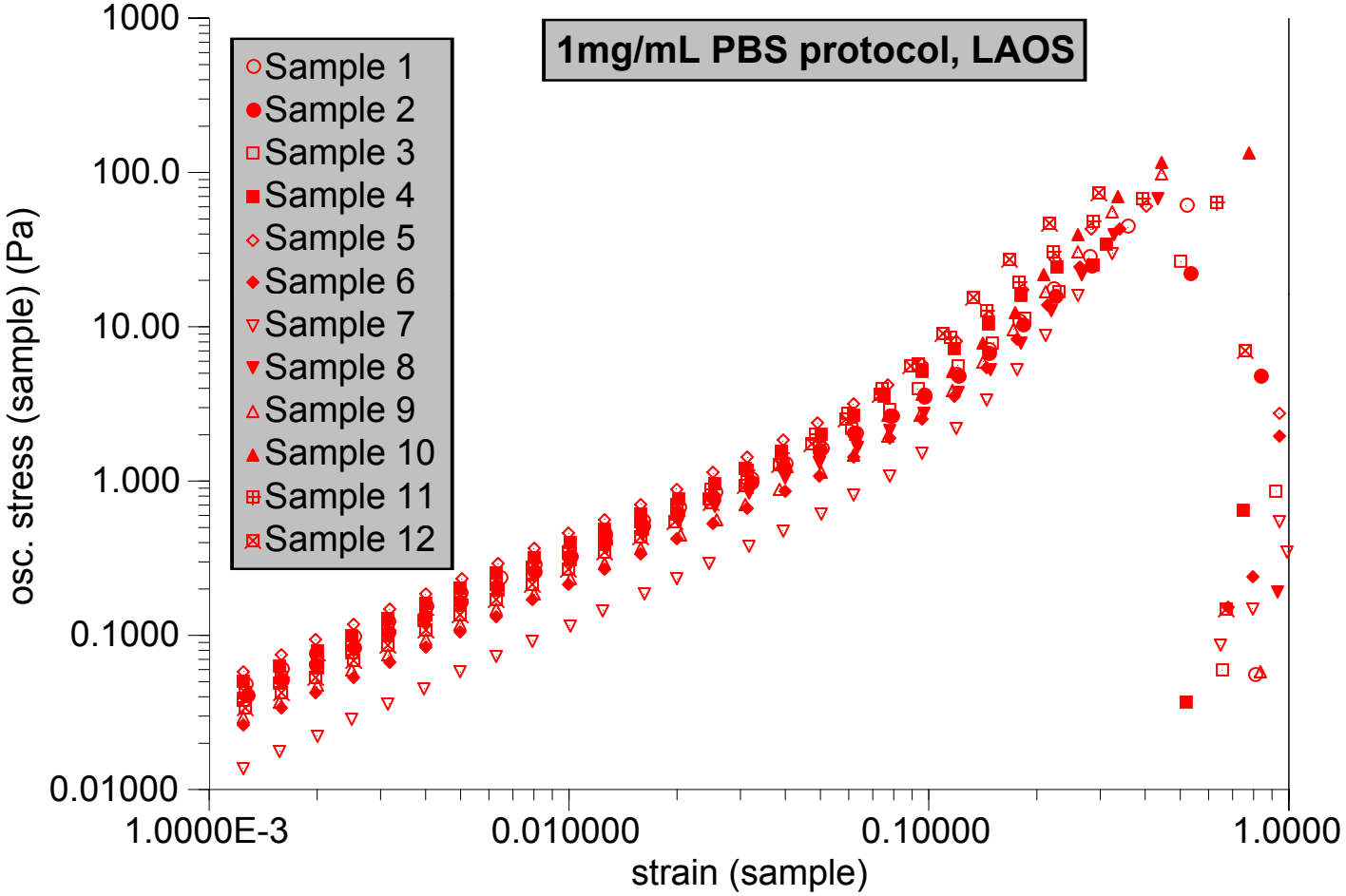
Collagen's creep response



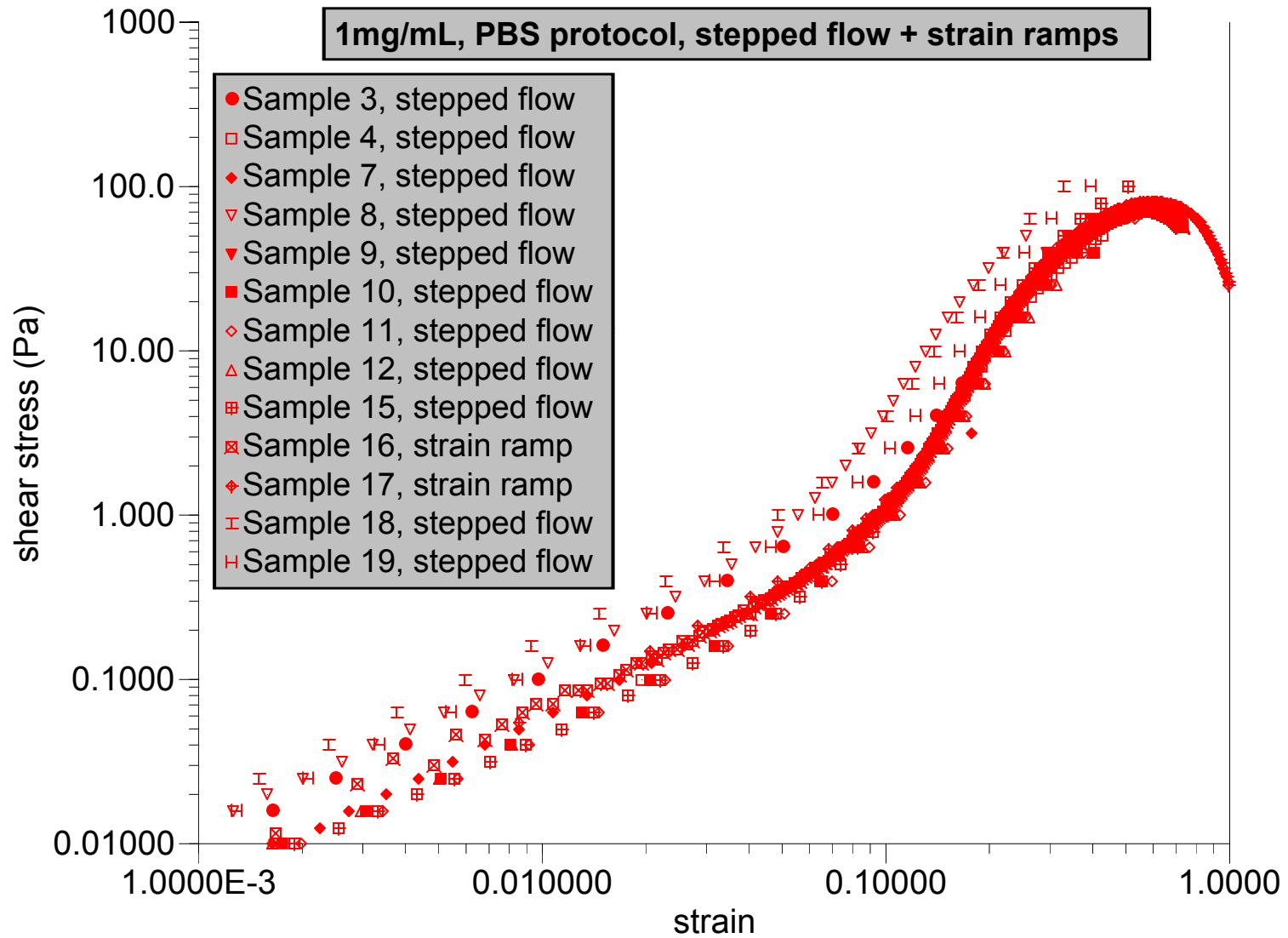
Creep-ringing results



Large amplitude oscillatory shear results

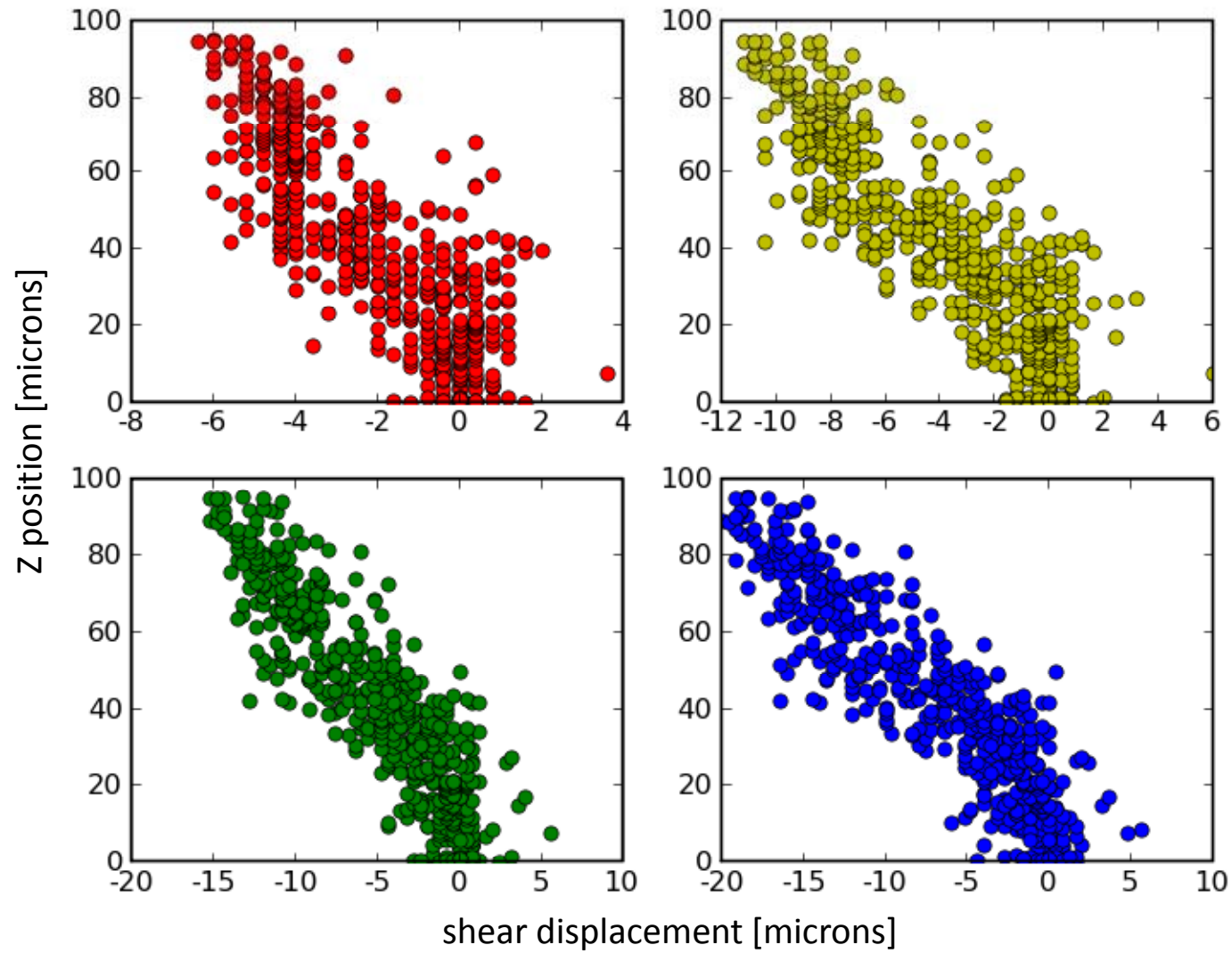


Creep-ringing results

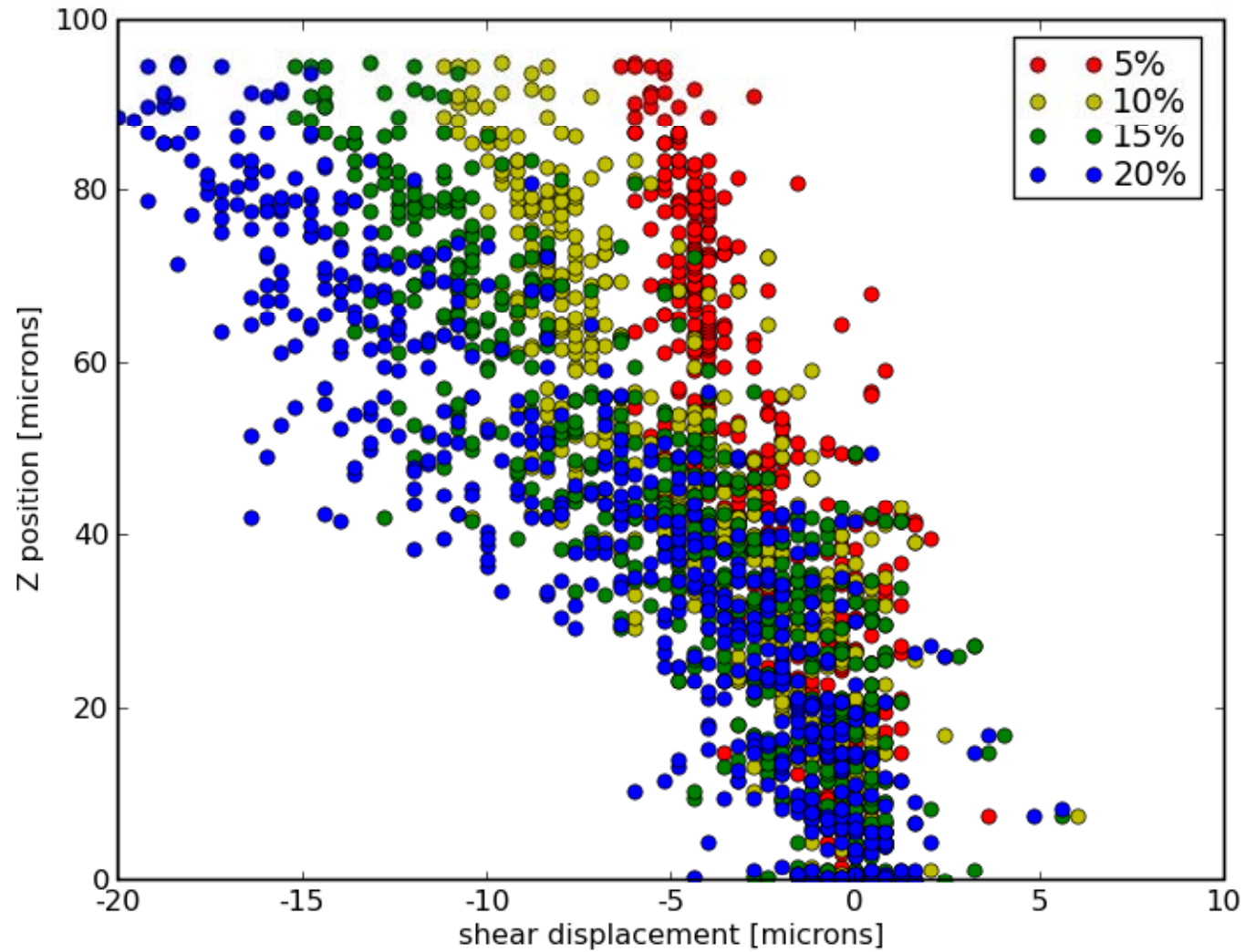


Origin of nonlinear behavior

Shear profiles

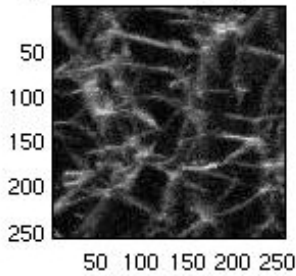


Shear profiles

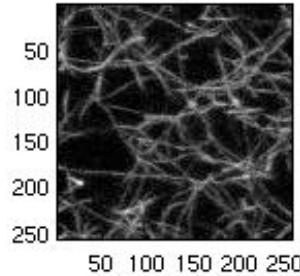


Geometrical properties

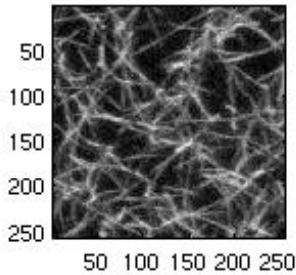
1.0mgmL: flattened image (zwid=20pix)



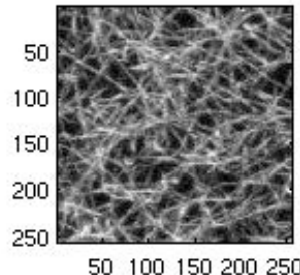
1.5mgmL



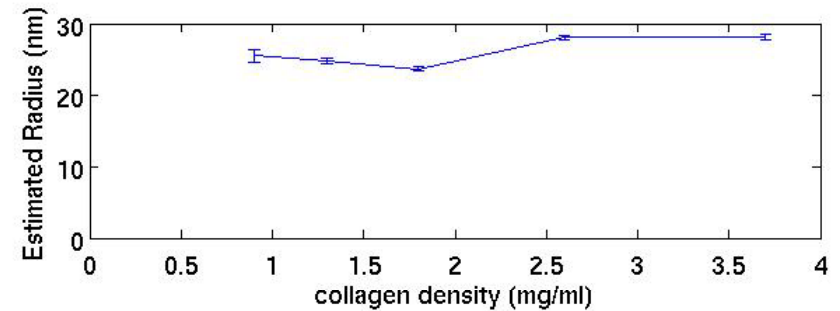
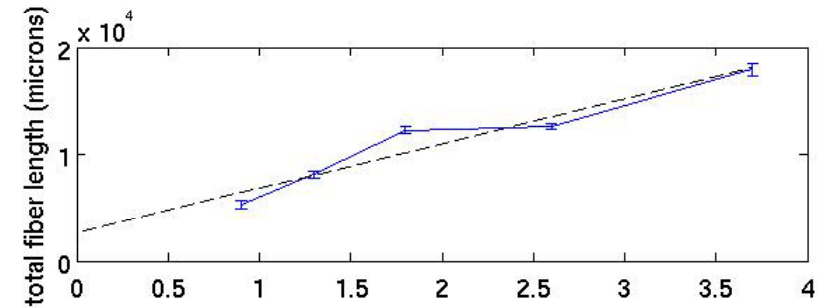
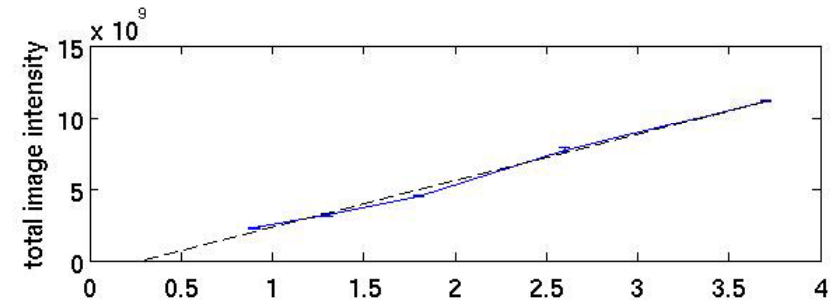
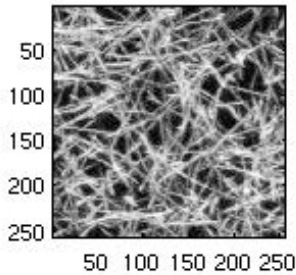
2.0mgmL



2.8mgmL



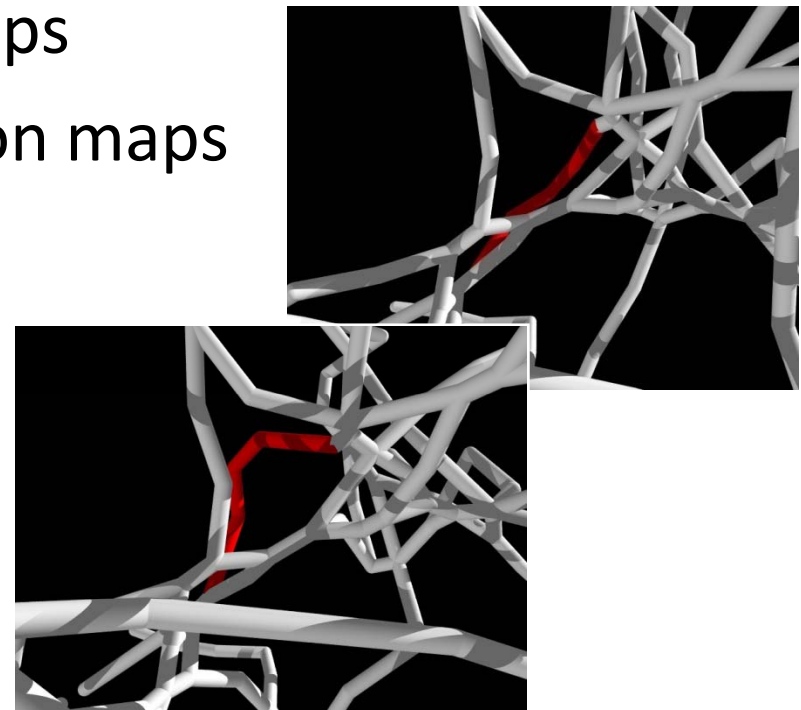
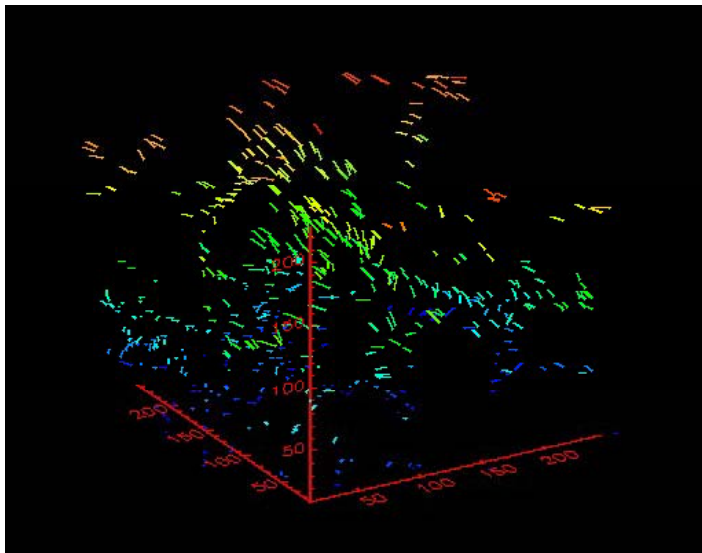
4.0mgmL



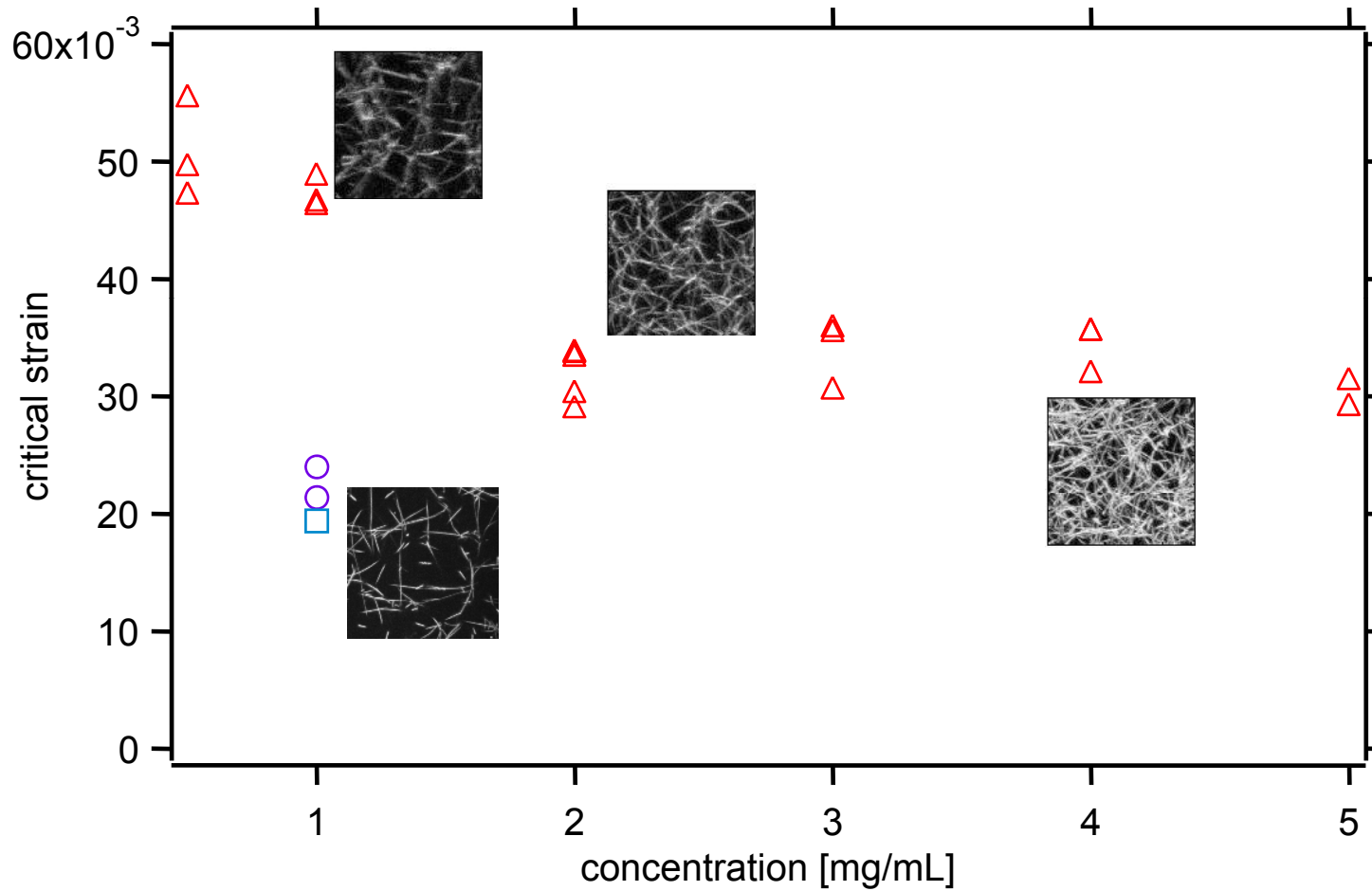
$0.2\mu\text{m}/\text{px} \Rightarrow 50\mu\text{m} \times 50\mu\text{m} \times 4\mu\text{m}$

Single fiber/xlink behavior

- Bio(polymer) Fi(ber) T(racking): BioFiT
 - Use fiber skeleton + raw image
 - Track fiber crosslinks => track fibers
 - Generate displacement maps
 - Generate fiber deformation maps

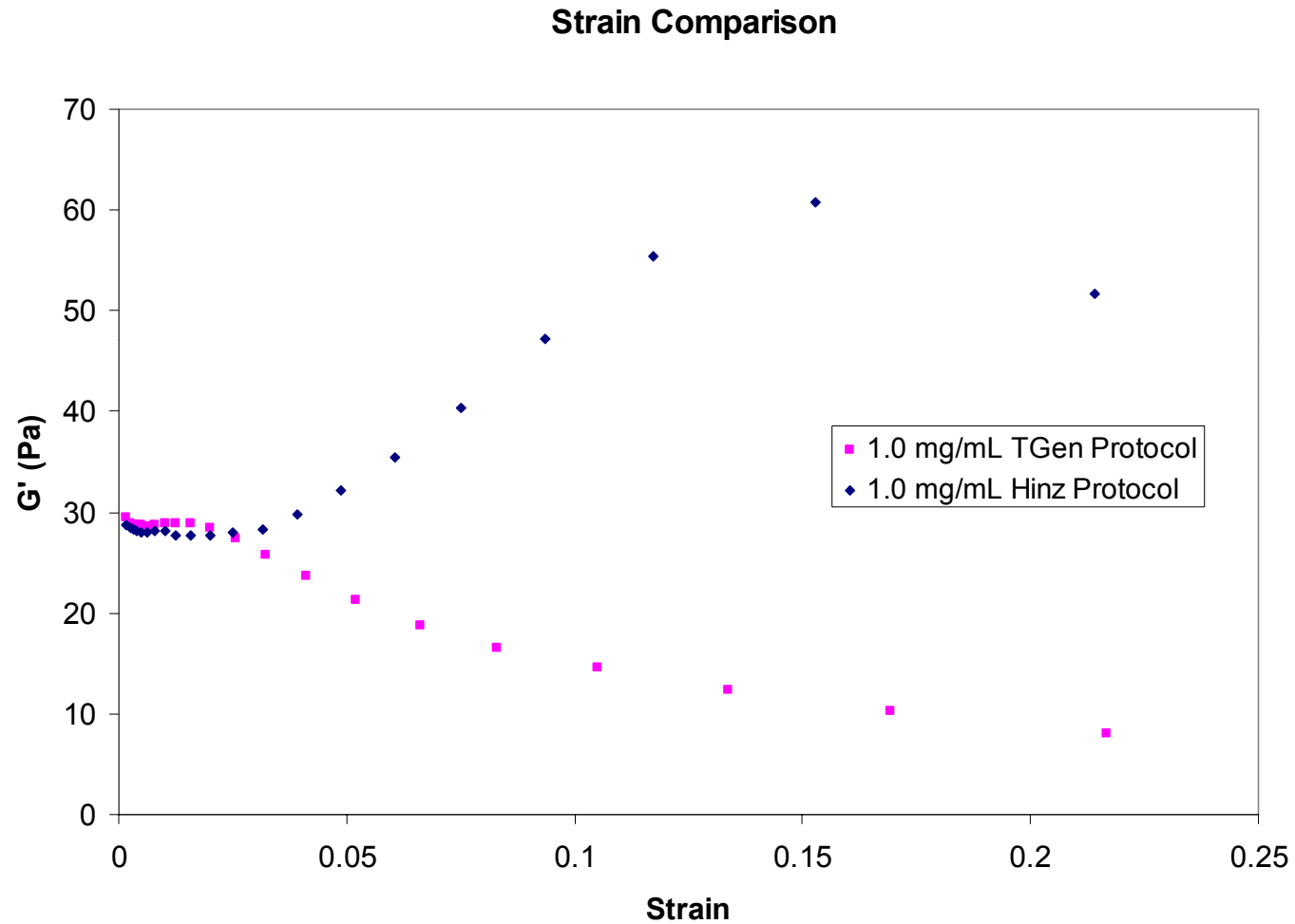


Onset of strain stiffening



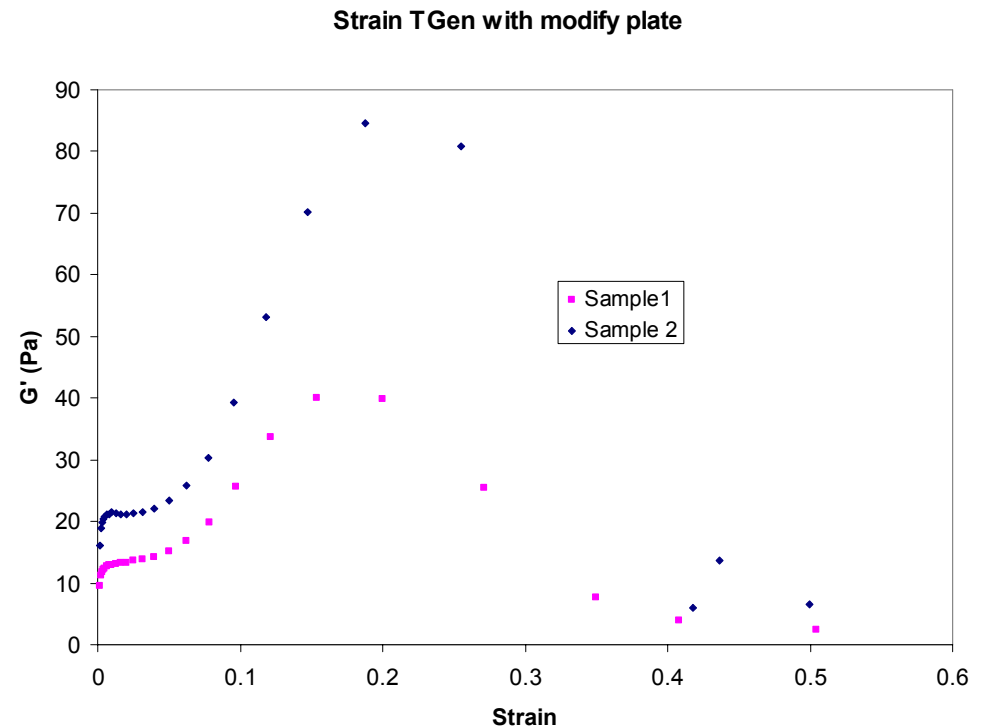
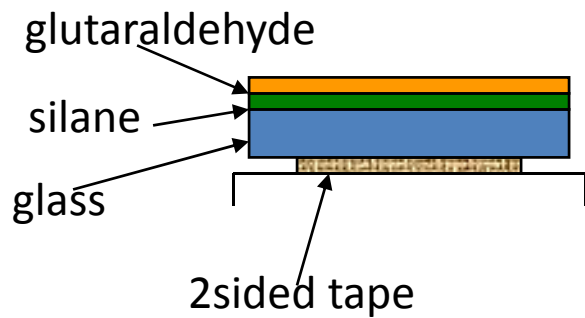
Probing surface attachment

Pablo: only one of the two protocols stiffens....

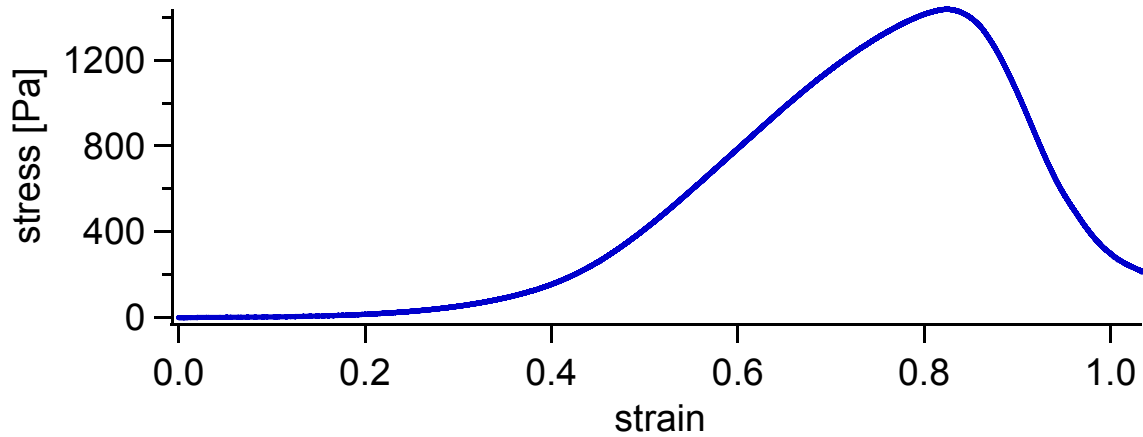
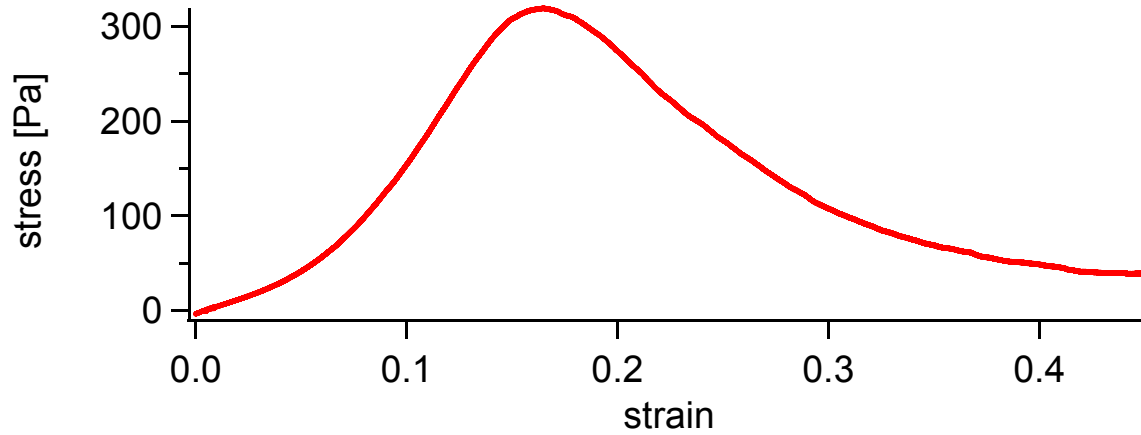


Pablo: but...

- We expect similar qualitative behavior between two protocols
- Are we really probing collagen mechanics OR surface attachment?

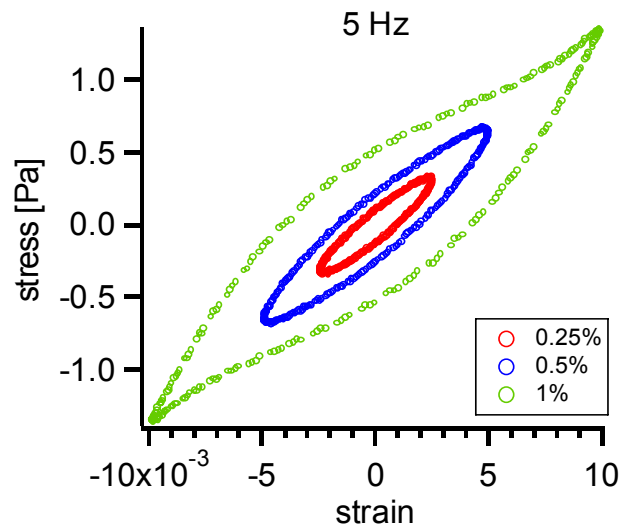
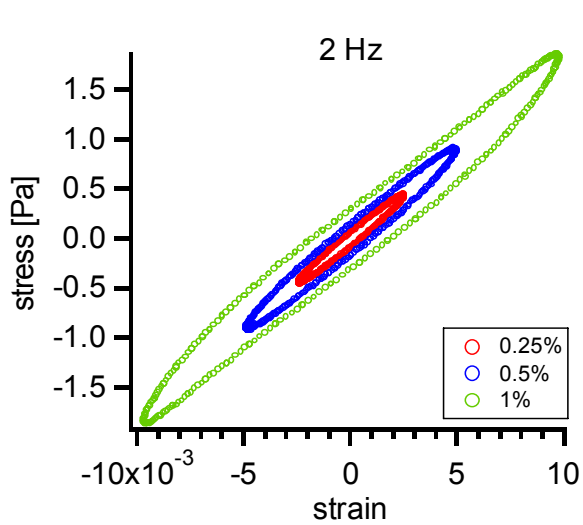
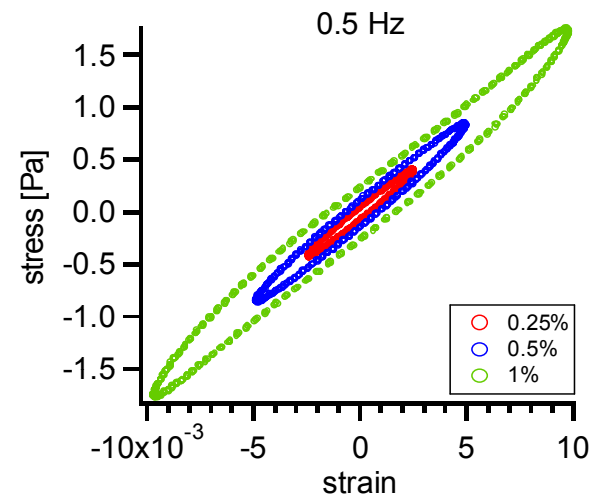
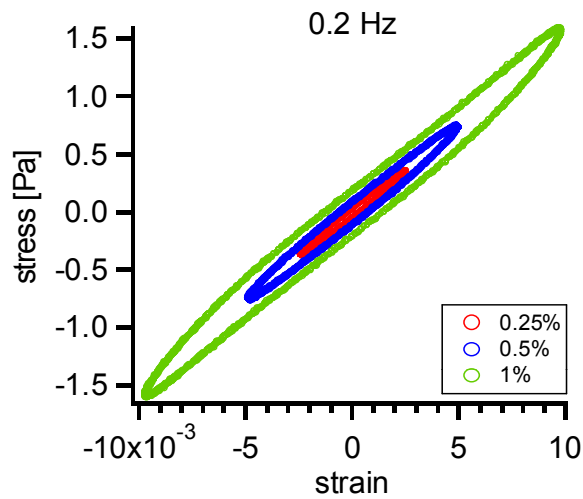
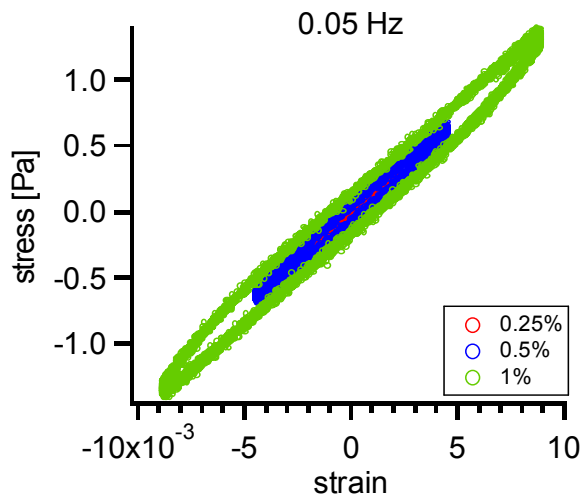


Sticking of top/bottom surface



More on LAOS

Strain rate dependence?



Nonlinear viscoelasticity (*Cho 2005*)

Important assumptions:

- periodicity, i.e. closed Lissajou curves
- steady-state, i.e. no plastic deformation

Time and frequency dependence implicit:

$$\sigma(\omega, \gamma_0, t) = \sigma(x, y)$$

Change of sign of strain =>

$$\sigma(-x, -y) = -\sigma(x, y)$$



$$\sigma(x, y) = \frac{\sigma(x, y) - \sigma(-x, y)}{2} + \frac{\sigma(x, y) - \sigma(x, -y)}{2}$$

$$\sigma_{OE} = \frac{\sigma(x, y) - \sigma(-x, y)}{2}, \quad \sigma_{EO} = \frac{\sigma(x, y) - \sigma(x, -y)}{2}$$

Parity =>

$$\oint \sigma_{OE} dx = 0 \quad \oint \sigma_{EO} dy = 0$$

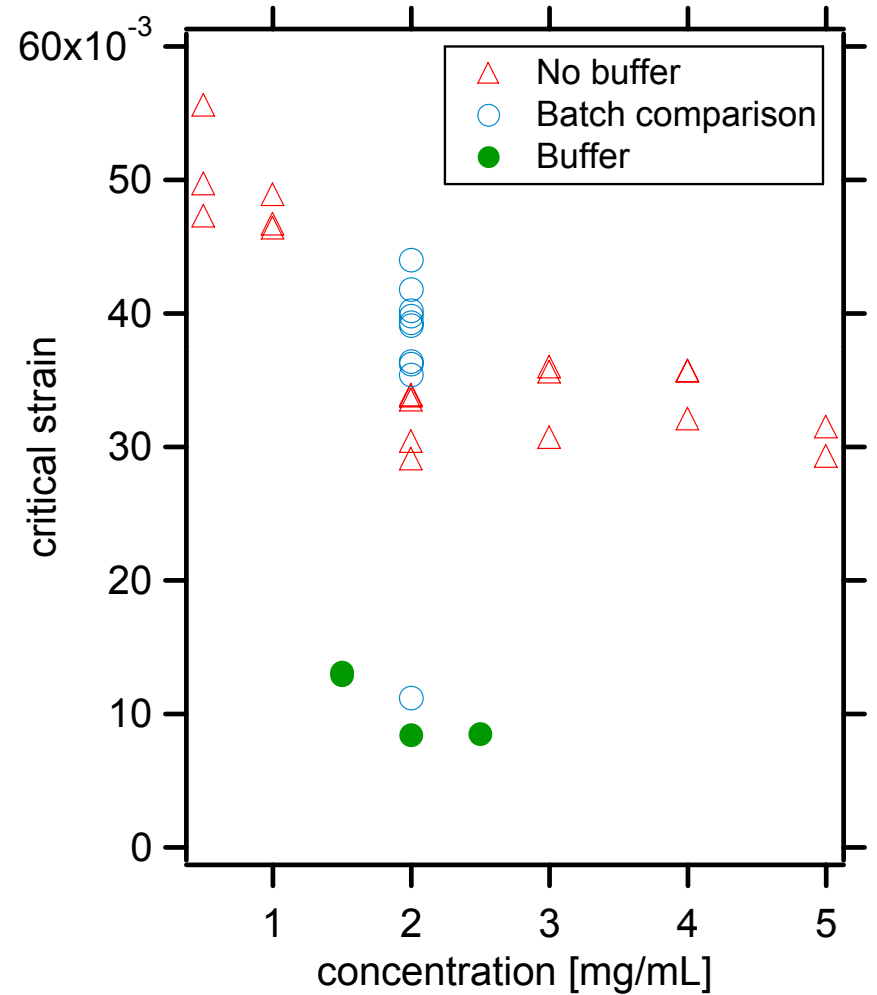
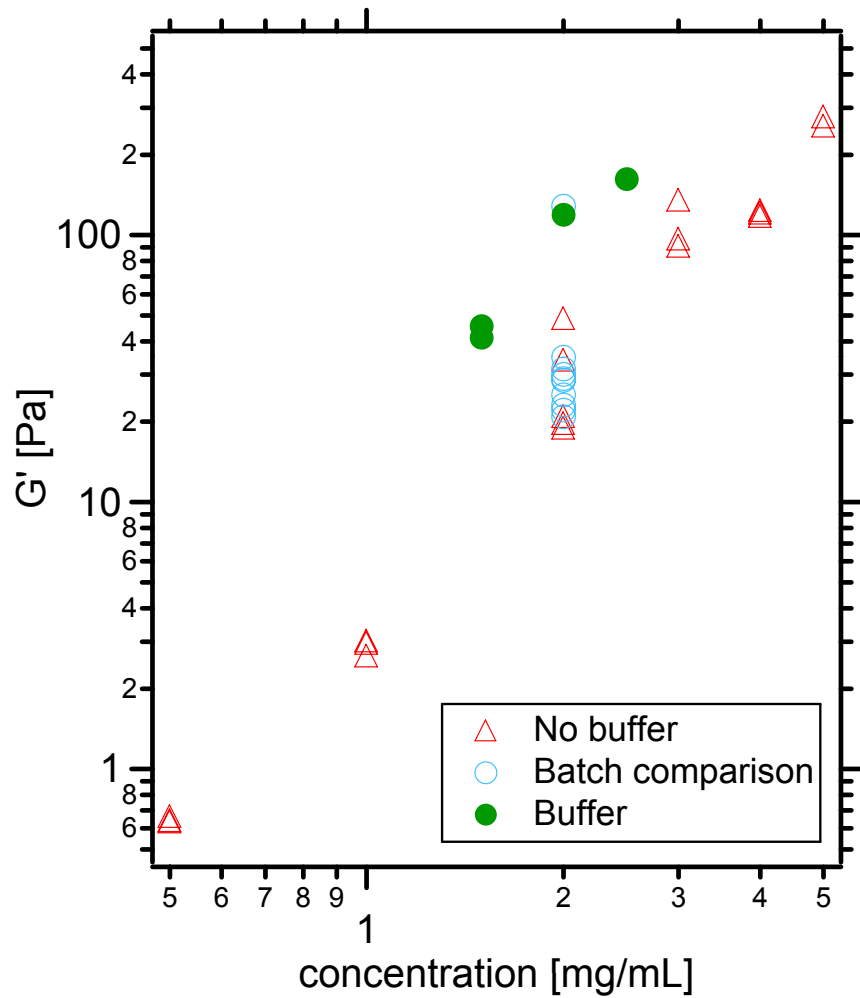
$$\oint \sigma dx = \oint \sigma_{EO} dx, \quad \oint \sigma dy = \oint \sigma_{OE} dy$$

Uniqueness?

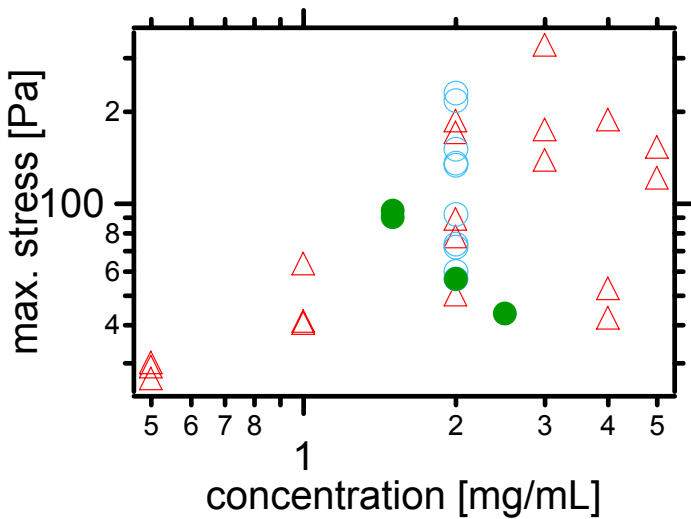
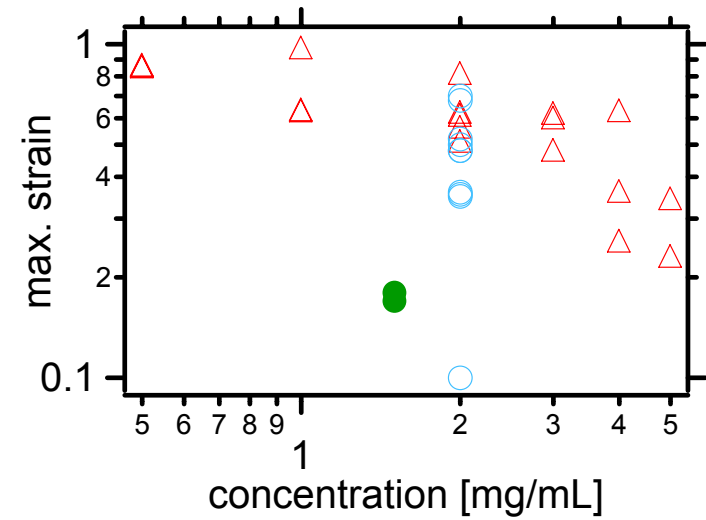
$$\sigma'(x, y) = \sigma'(x, \gamma_0), \quad \sigma''(x, y) = \sigma''(y, \gamma_0)$$

Rheology results

Modulus and γ_{crit}



Other variables of interest?



K' calculated as derivative of stress-strain curve

